

Raster **I**mage **C**orrelation **S**pectroscopy **RICS**

Novel Idea: **R**aster **I**mage **C**orrelation **S**pectroscopy

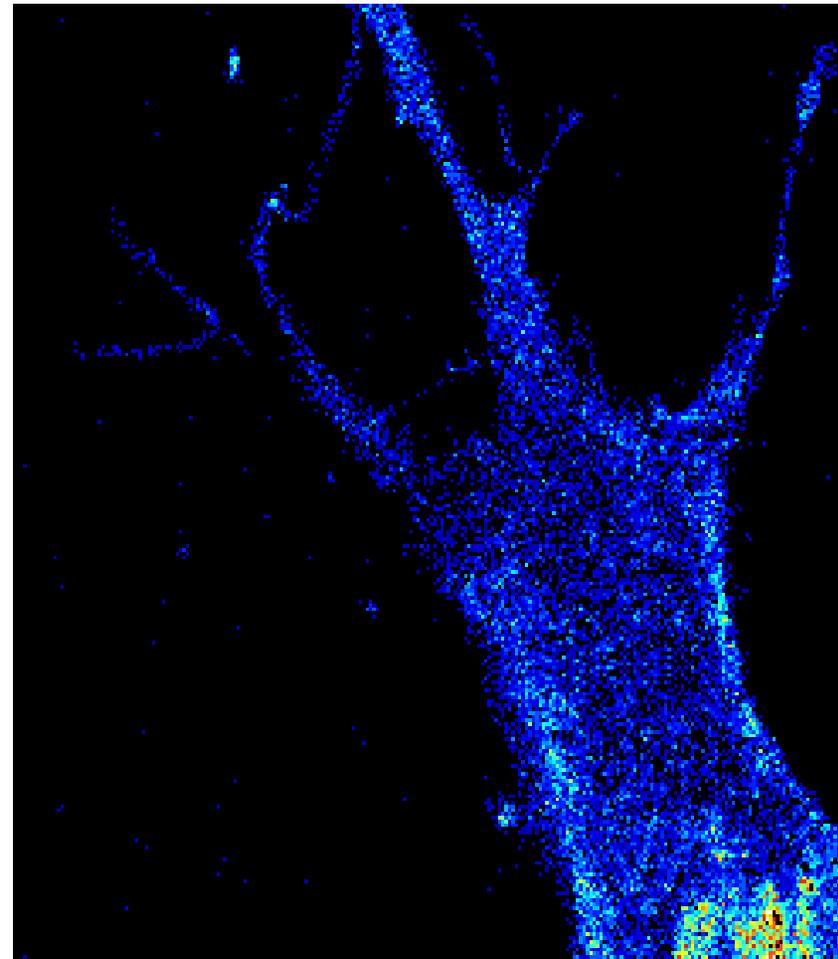
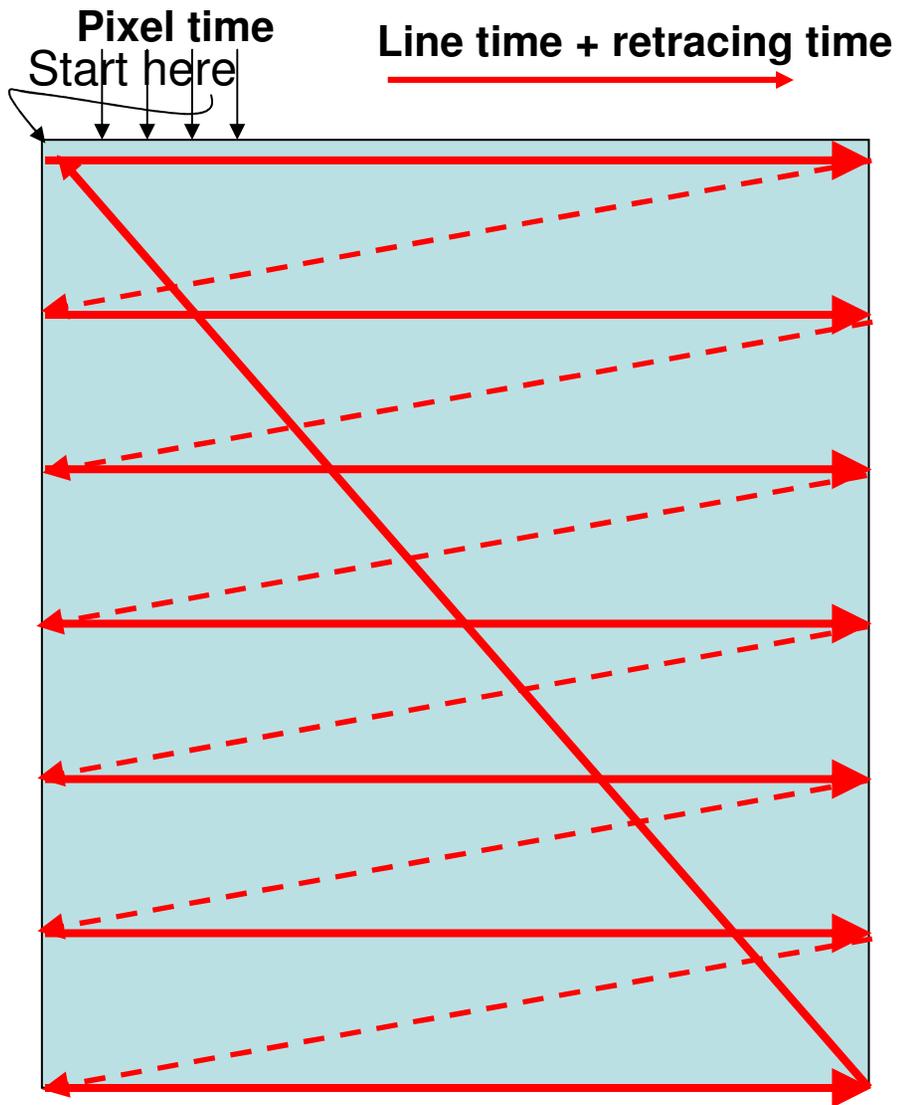
We can have a combination of very high time resolution with sufficient spatial resolution.

Major benefits of RICS:

- It can be done with **commercial laser scanning microscopes** (either one or two photon systems)
- It can be done with **analog detection**, as well as with photon counting systems, although the characteristic of the detector must be accounted for (time correlations at very short times due to the analog filter)
- RICS provides an intrinsic method to separate the immobile fraction
- It provides a powerful method to distinguish diffusion from binding

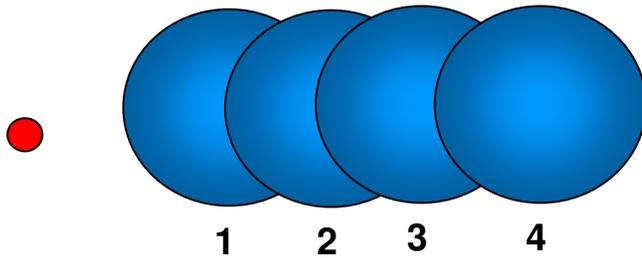
How does it work?

Raster Scanning

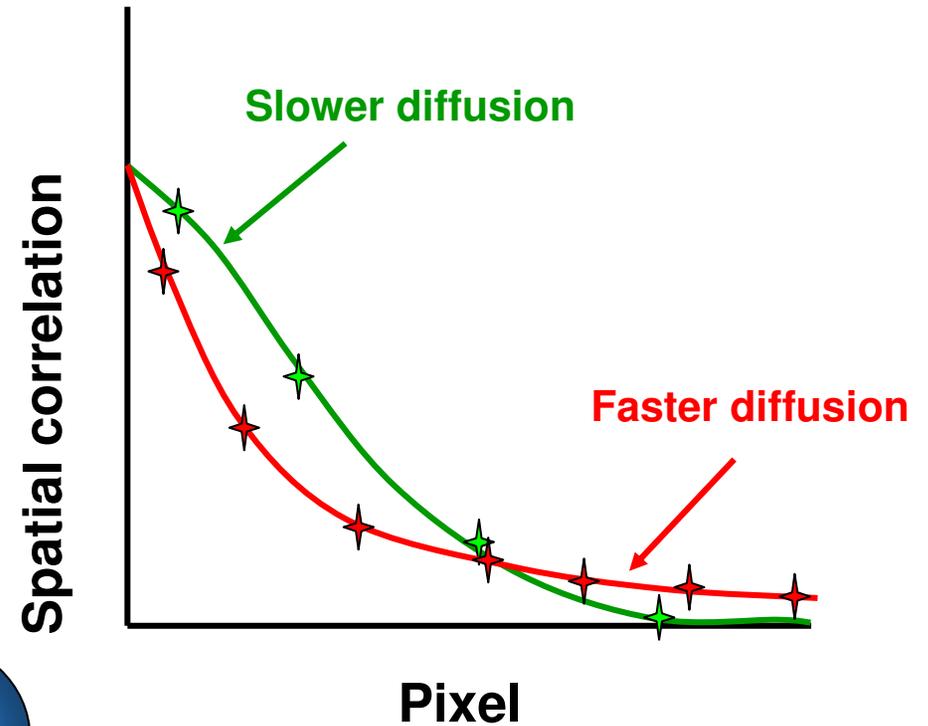
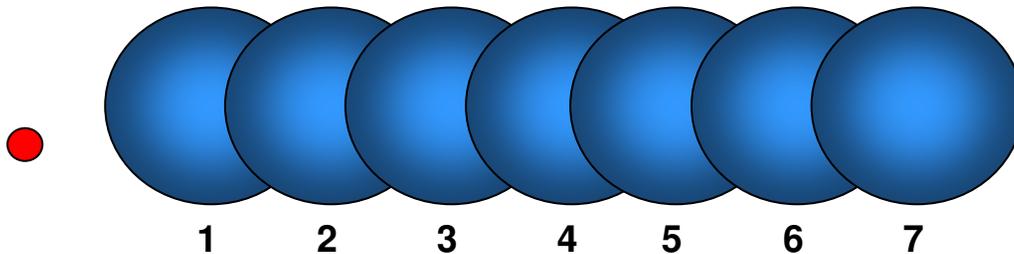


Temporal information hidden in the raster-scan image: the RICS approach

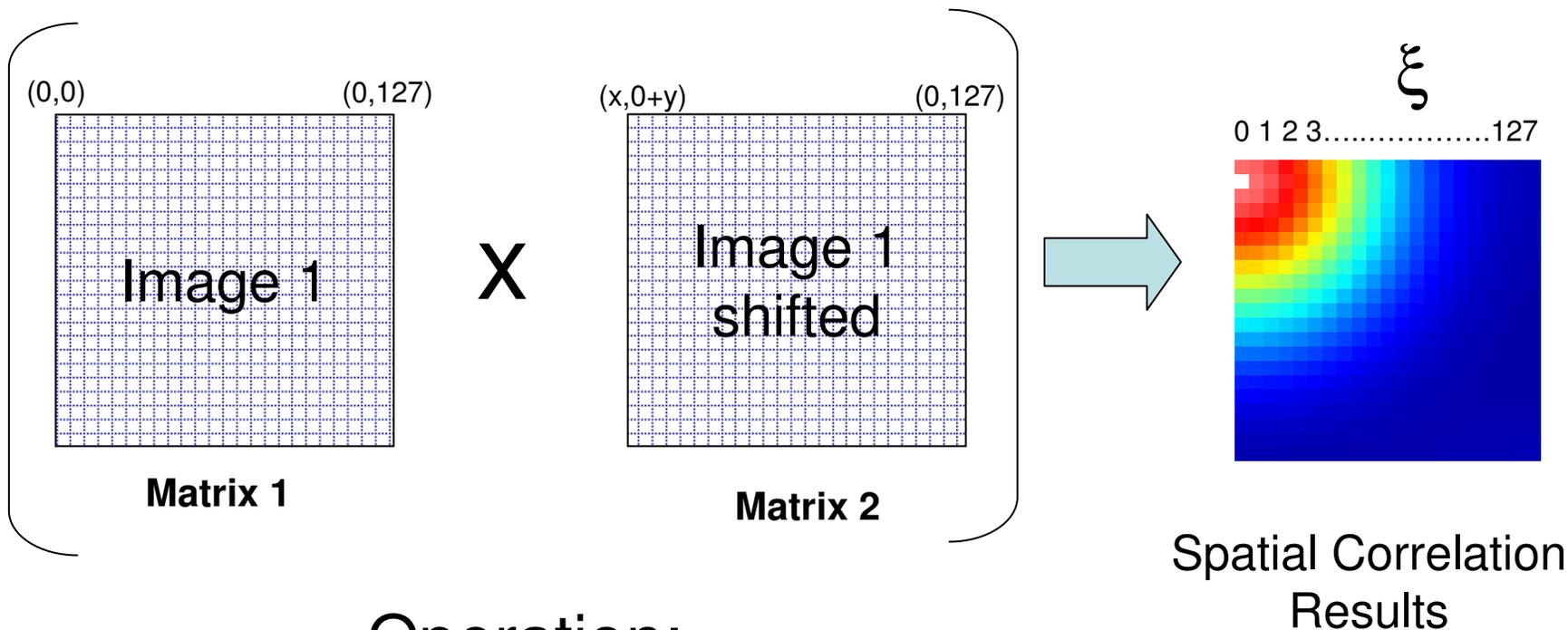
Situation 1: slow diffusion



Situation 2: fast diffusion



How is the spatial correlation done?



Operation:

In the x direction

PLUS In the y direction

$$(0,0 \times 0,0) + (0,1 \times 0,1) + (0,2 \times 0,2) \dots (0,127 \times 0,127) \\ + (1,0 \times 1,0) + (1,1 \times 1,1) + (1,2 \times 1,2) \dots (1,127 \times 1,127)$$

One number is obtained for x and y and is divided by the average intensity squared

The RICS approach: 2-D spatial correlations

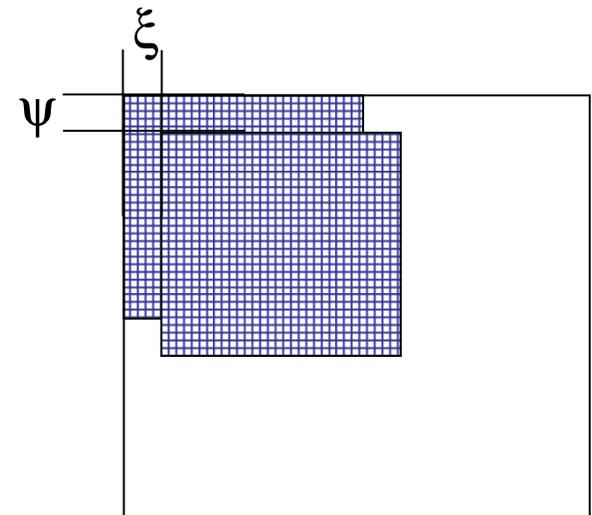
In a raster-scan image, points are measured at different positions and at different times simultaneously

If we consider the **time sequence**, it is not continuous in time

If we consider the **pixel sequence**, it is contiguous in space

In the RICS approach we calculate the 2-D spatial correlation function (similarly to the ICS method of Petersen and Wiseman)

$$G_{RICS}(\xi, \psi) = \frac{\langle I(x, y)I(x + \xi, y + \psi) \rangle}{\langle I(x, y) \rangle^2}$$



The variables **x** and **y** represent spatial increments in the **x** and **y** directions, respectively

2-D spatial correlation can be computed very efficiently using FFT methods.

To introduce the “RICS concept” we must account for the relationship between time and position of the scanning laser beam.

The RICS approach for diffusion

The the dynamics at a point is independent on the scanning motion of the laser beam

$$G_{RICS}(\xi, \psi) = S(\xi, \psi) \times G(\xi, \psi)$$

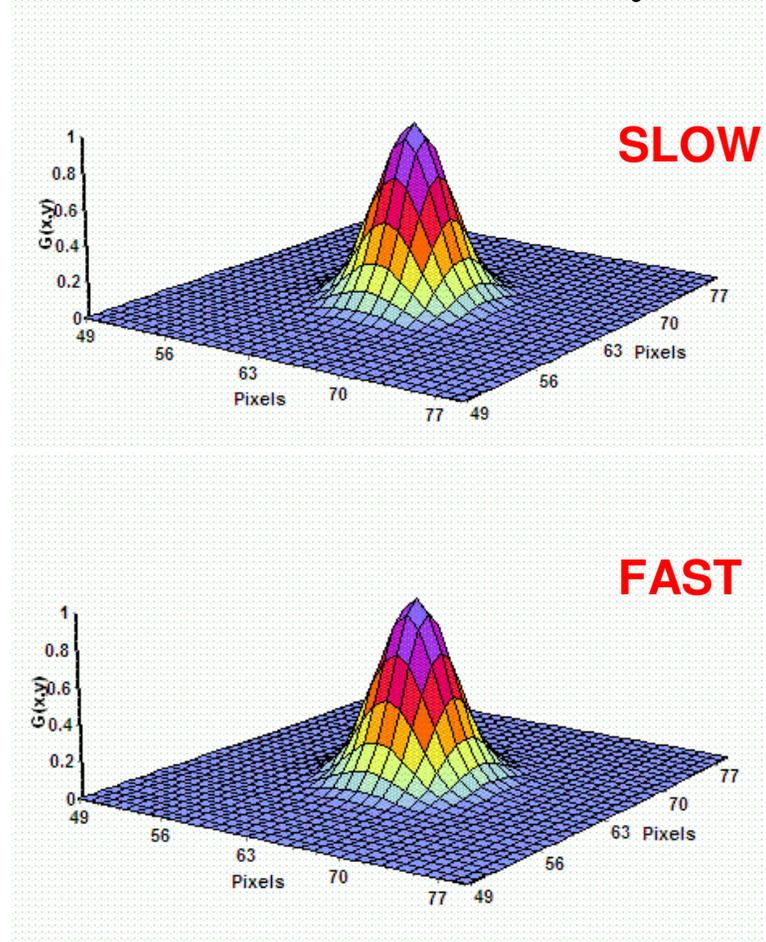
Consider now the process of diffusion. The diffusion kernel can be described by the following expression

$$P(r, t) = \frac{1}{(4\pi Dt)^{3/2}} \exp\left(-\frac{r^2}{4Dt}\right)$$

There are two parts:

- (1) the temporal term,
- (2) the spatial Gaussian term

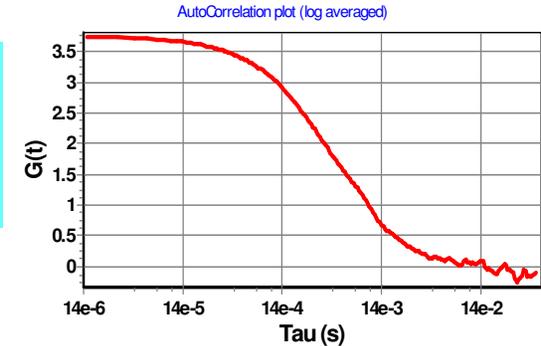
For any diffusion the amplitude decreases as a function of time and the width of the Gaussian increases as a function of time



RICS: space and time relationships

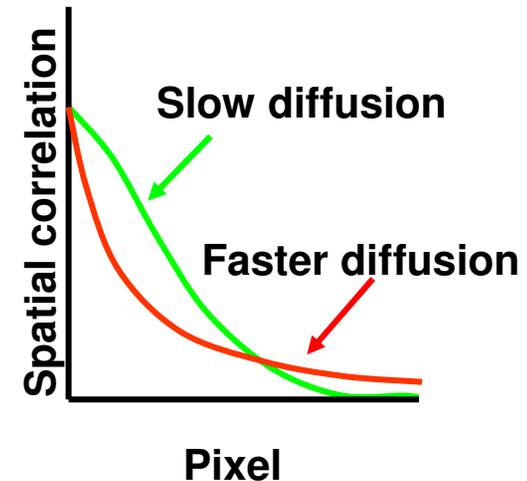
At any position, the ACF due to diffusion takes the familiar form:

$$G(\xi, \psi) = \frac{\gamma}{N} \left(1 + \frac{4D(\tau_p \xi + \tau_l \psi)}{w_0^2} \right)^{-1} \left(1 + \frac{4D(\tau_p \xi + \tau_l \psi)}{w_z^2} \right)^{-1/2}$$



τ_p and τ_l indicate the pixel time and the line time.
The correlation due to the scanner movement is:

$$S(\xi, \psi) = \exp \left(- \frac{\left[\left(\frac{2\xi \delta r}{w_0} \right)^2 + \left(\frac{2\psi \delta r}{w_0} \right)^2 \right]}{\left(1 + \frac{4D(\tau_p \xi + \tau_l \psi)}{w_0^2} \right)} \right)$$



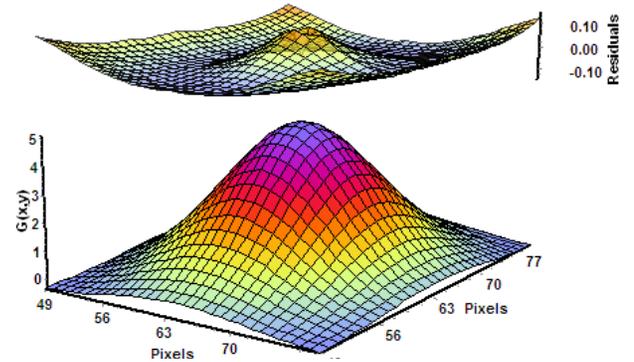
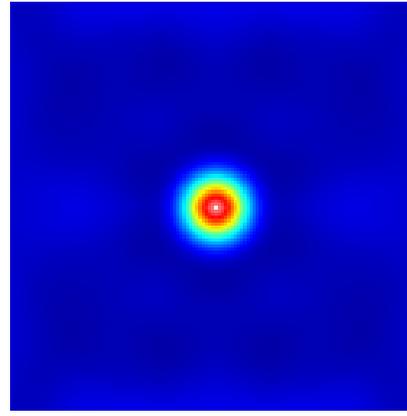
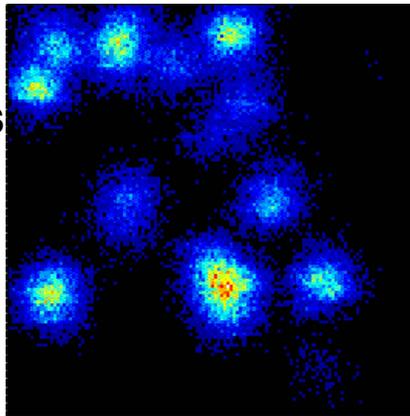
Where δr is the pixel size. For $D=0$ the spatial correlation gives the autocorrelation of the PSF, with an amplitude equal to γ/N . As D increases, the correlation (G term) becomes narrower and the width of the S term increases.

RICS Simulations of three different diffusion rates:

Box size=3.4 μm sampling time: 1) 32 μs /pixel 2) 8 μs /pixel 3) 4 μs /pixel

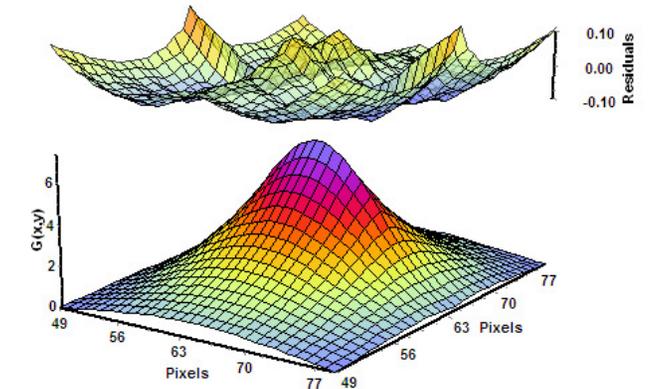
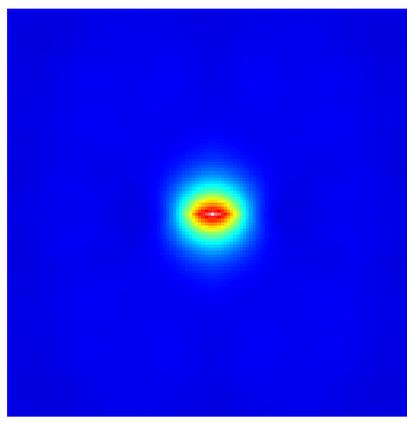
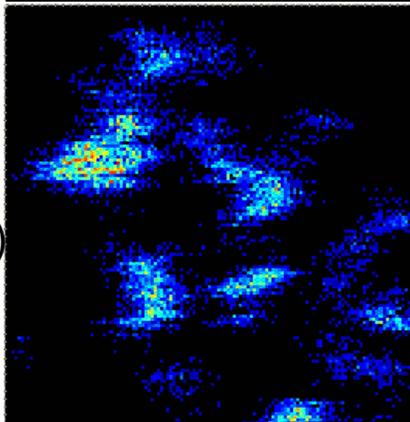
$D = 0.1 \mu\text{m}^2/\text{s}$

(membrane proteins)



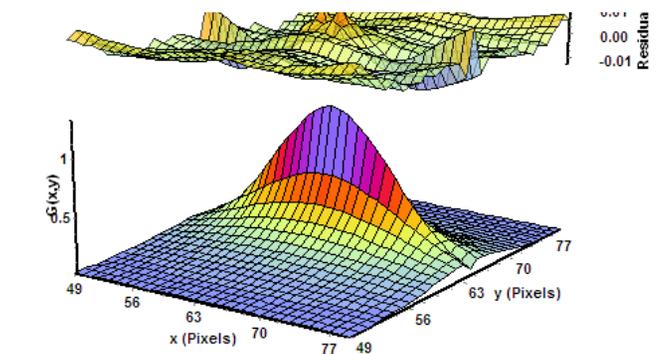
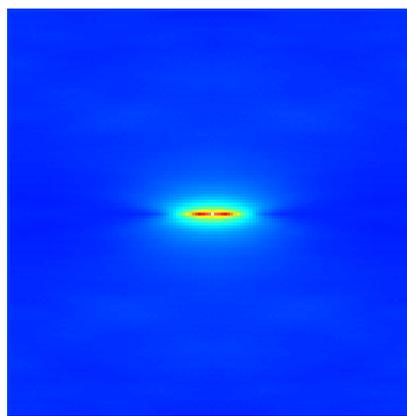
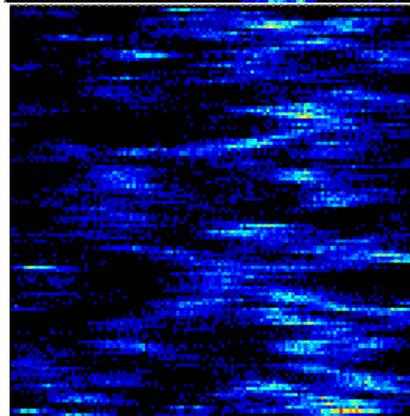
$D = 5.0 \mu\text{m}^2/\text{s}$

(40 nm beads)



$D = 90 \mu\text{m}^2/\text{s}$

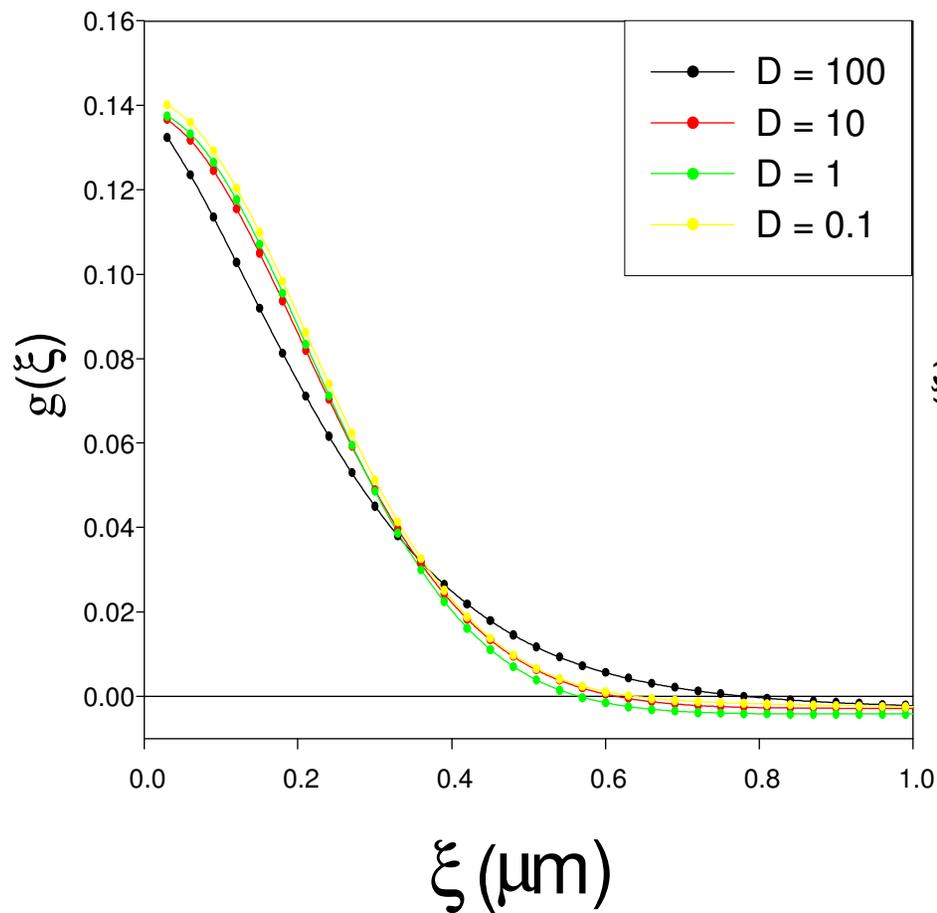
(EGFP)



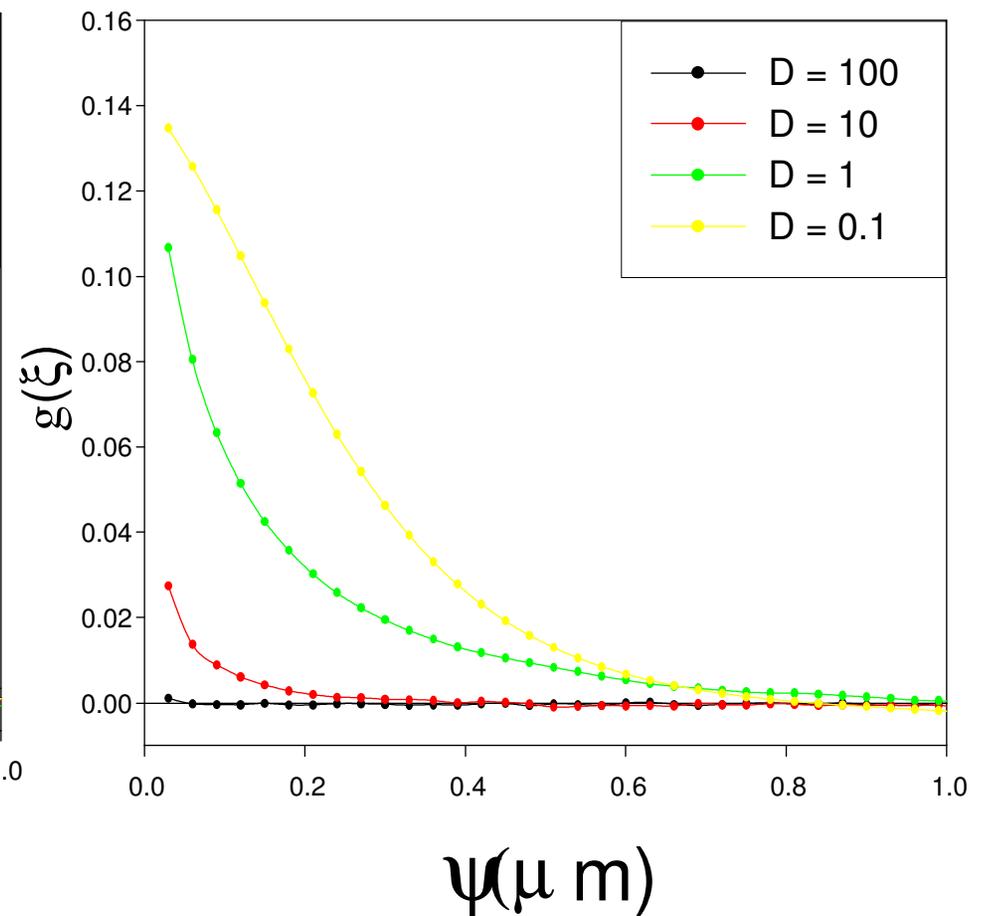
Horizontal and Vertical fits:

Simulations of beads 300 frames, 128x128pixels, 8 μ s/pix, size of pixels=30nm

Horizontal ACF



Vertical ACF



In SIMFCS

How to Setup the **Laser Scanning Confocal Microscope**

➤ **Scan Speeds ($\mu\text{s}/\text{pixel}$):**

- $4\mu\text{s}$ for fast molecules $D > 100\mu\text{m}^2/\text{s}$
- $8 - 32\mu\text{s}$ for slower molecules $D = 1\mu\text{m}^2/\text{s} - 100\mu\text{m}^2/\text{s}$
- $32 - 100\mu\text{s}$ for slower molecules $D = 0.1\mu\text{m}^2/\text{s} - 10\mu\text{m}^2/\text{s}$

➤ **Pixel Size:**

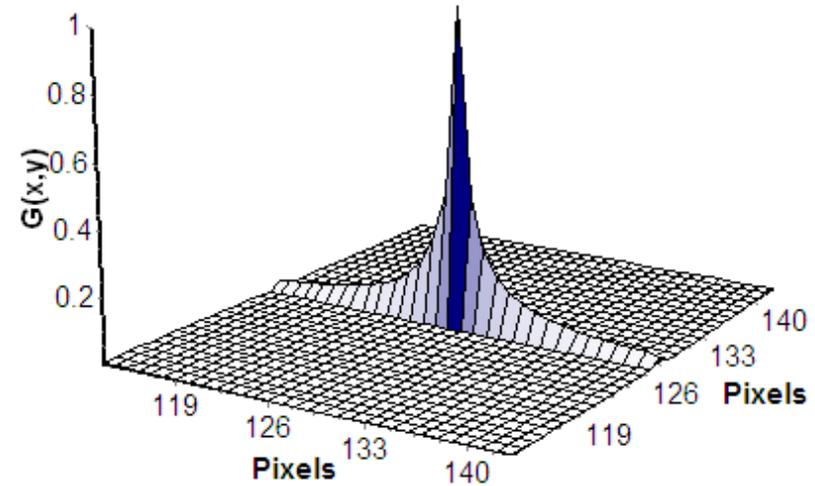
- 3-4x smaller than the Point Spread Function (PSF) $\approx 300\text{nm}$

➤ **Molecular Concentrations**

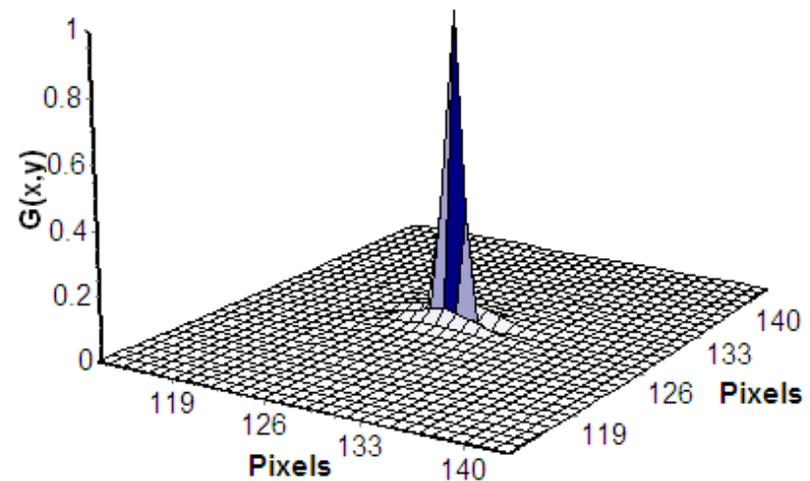
- Same conditions as conventional FCS methods

Common Errors in RICS

Scanning Too Slow
(100 $\mu\text{s}/\text{pixel}$, $D = 300 \mu\text{m}^2/\text{s}$)



Pixels are separated too much
relative to PSF
(pixel size = $w_0 = 0.3 \mu\text{m}$)

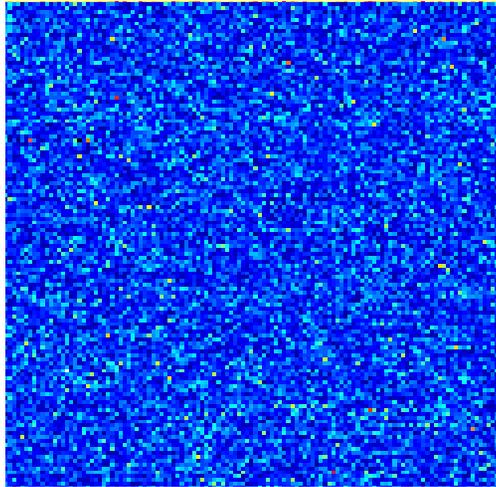


Courtesy of Jay Unruh

RICS: Fits to spatial correlation functions

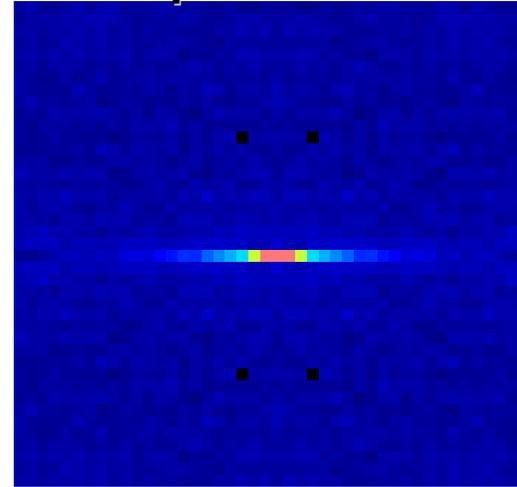
Olympus Fluoview300 LSM

EGFP in solution

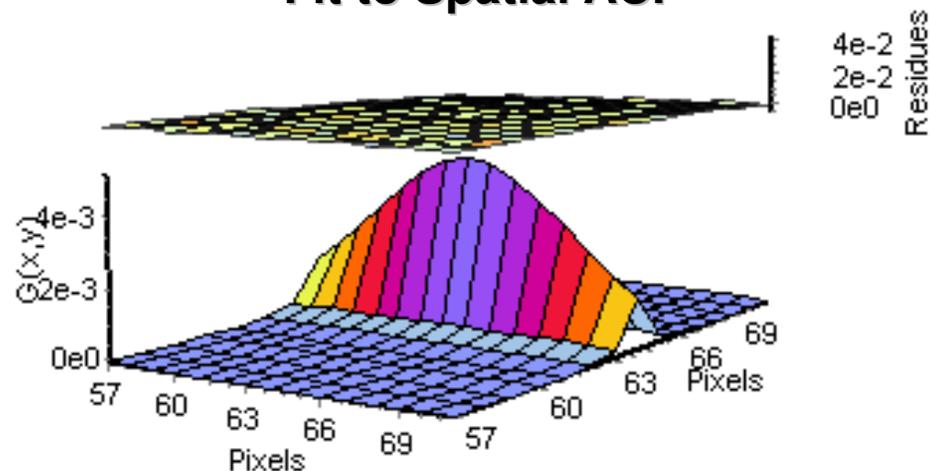


128x128, 4 $\mu\text{s}/\text{pixel}$, 5.4 ms/line, 0.023 $\mu\text{m}/\text{pixel}$

Spatial ACF

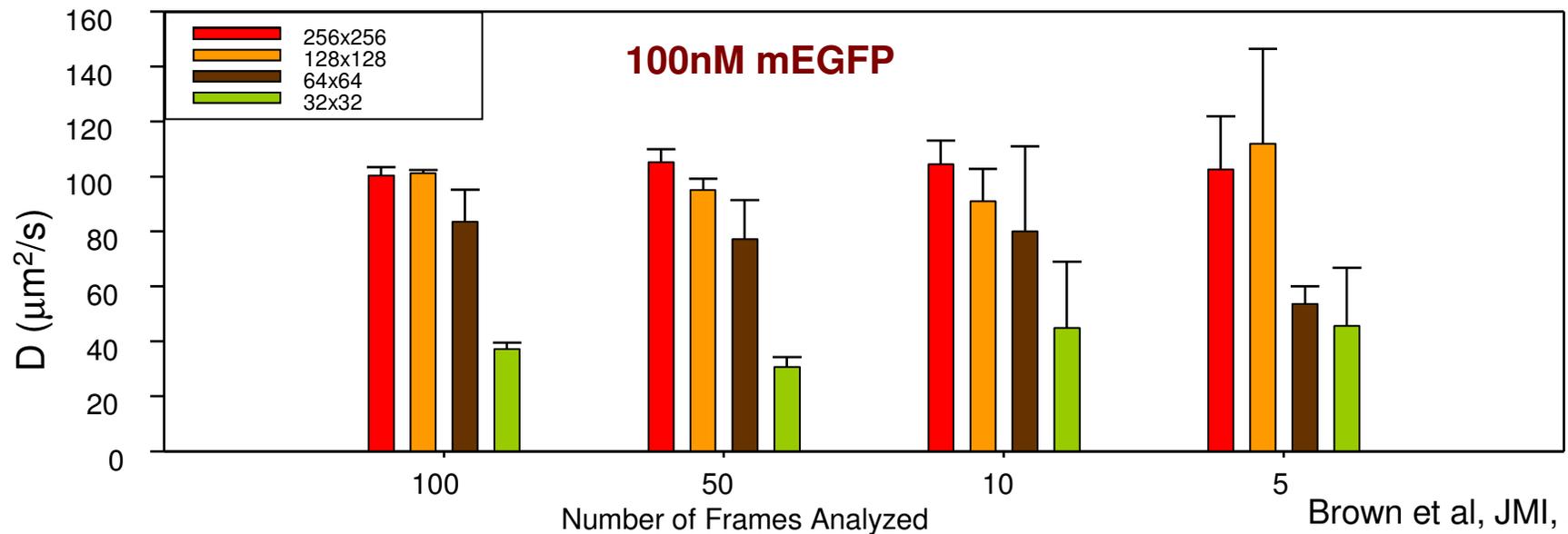
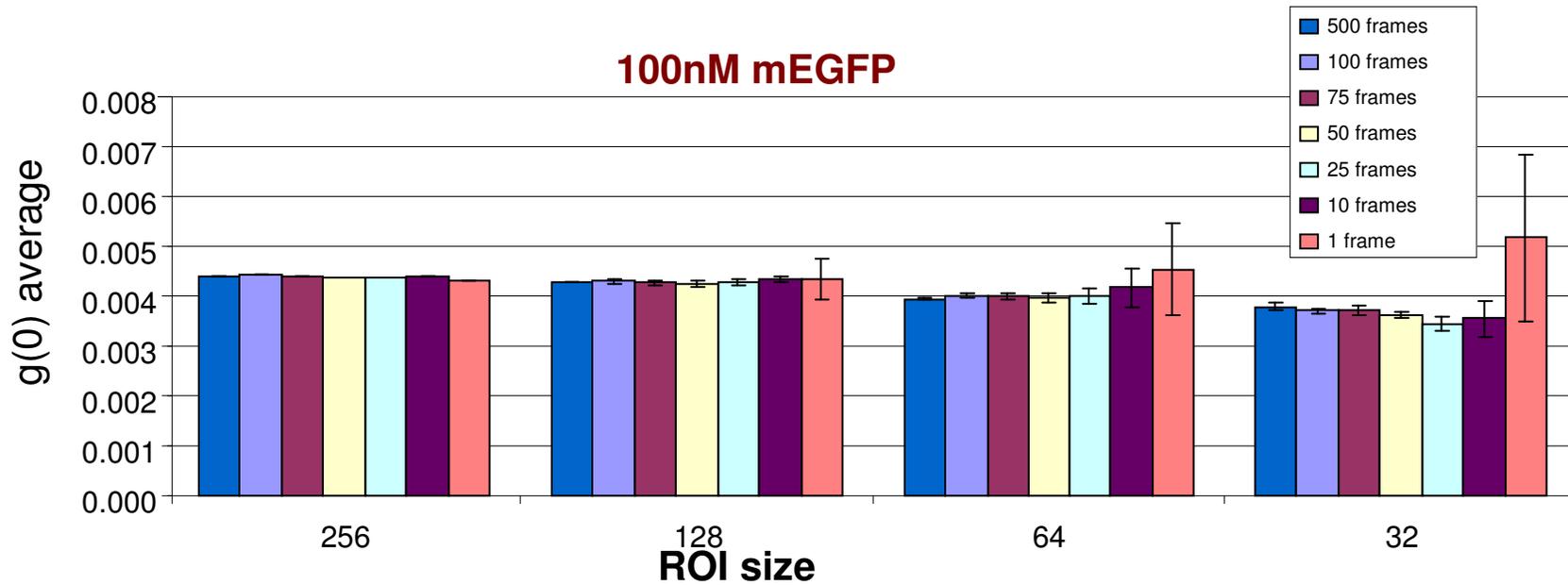


Fit to Spatial ACF

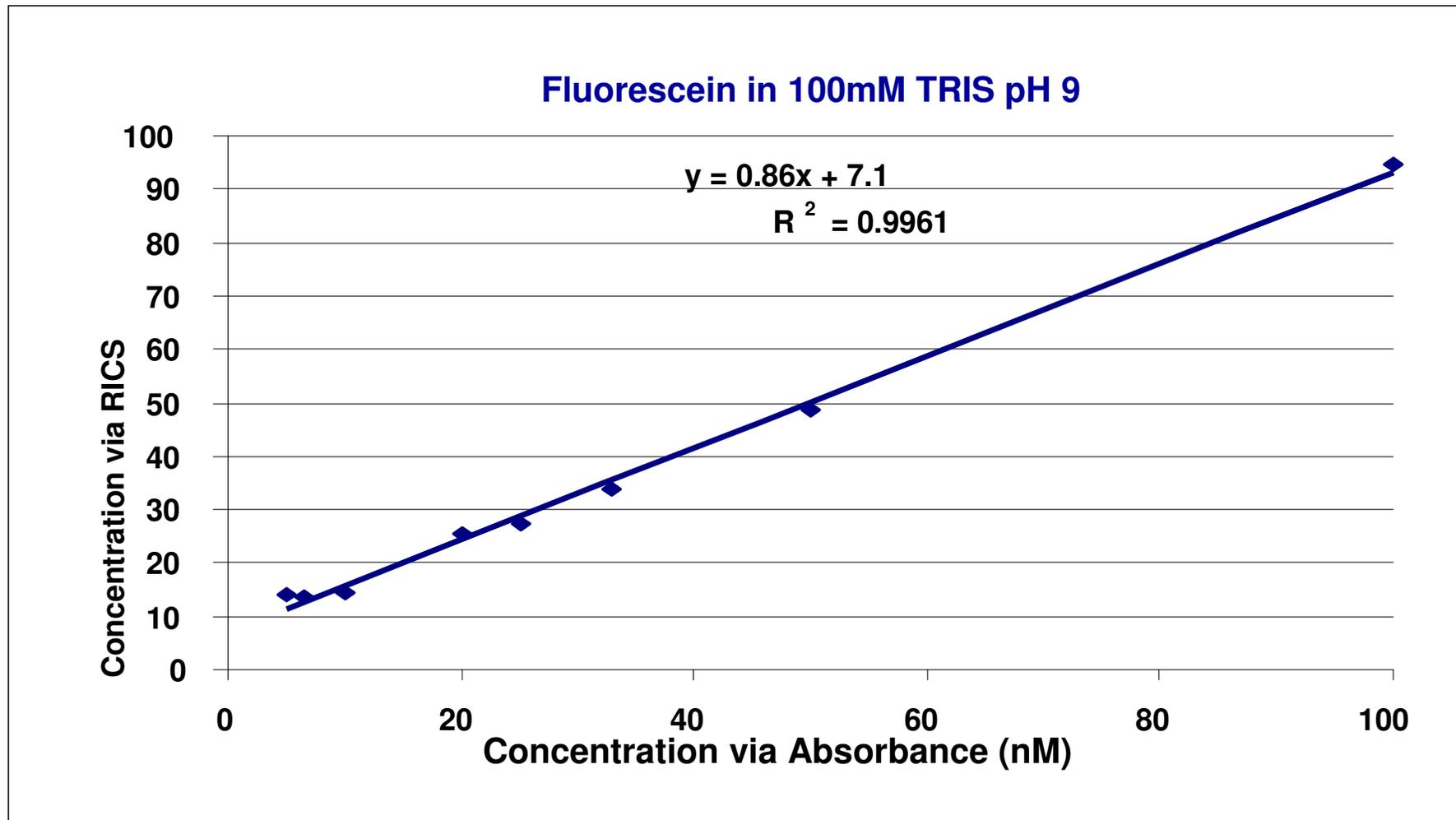


$$D = 105 \pm 10 \mu\text{m}^2/\text{s}$$

What ROI size to use? How many frames to acquire?



Obtaining concentration from RICS



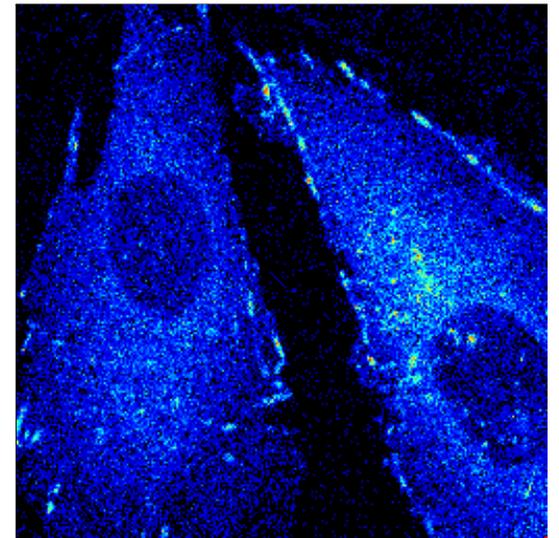
How we go from solutions to cells?

In cells we have an **immobile fraction**

The 2-D-spatial correlation of an image containing immobile features has a very strong correlation pattern

We need to separate this **immobile** fraction from the mobile part before calculating the transform

How is this achieved?



Does noise from the detectors correlate?

In a “truly immobile” bright region, the intensity fluctuates according to the Poisson distribution due to shot noise.

The time correlation of the shot noise is zero, except at time zero.

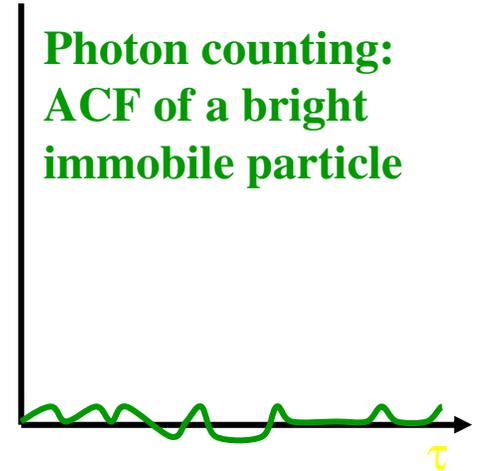
The spatial correlation of the intensity at any two pixels due to shot noise is zero, **even if the two points are within the PSF.**

If we subtract the average intensity and disregard the zero time-space point, the immobile bright region **totally disappear** from the correlation function

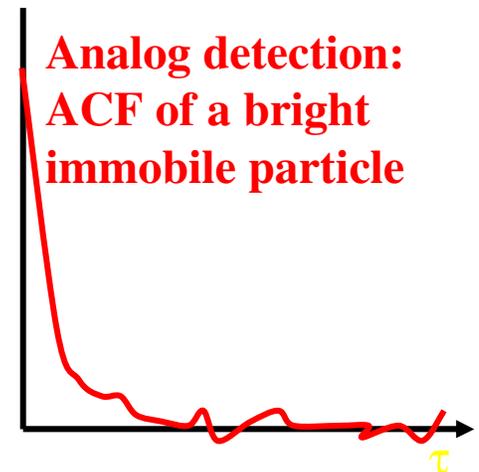
Attention!!!!

This is not true for analog detection, not even in the first order approximation. For analog detection the shot noise is time (and space) correlated.

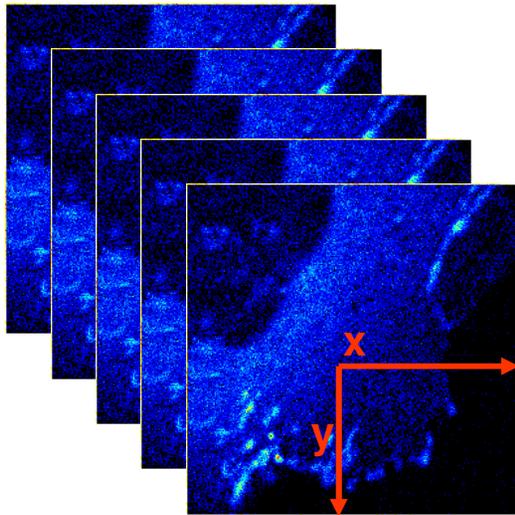
Photon counting:
ACF of a bright
immobile particle



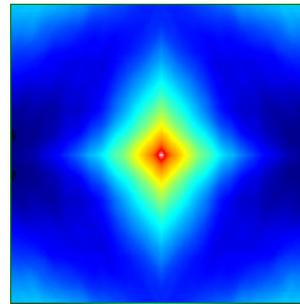
Analog detection:
ACF of a bright
immobile particle



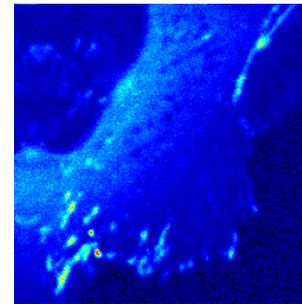
Formula used to subtract background:



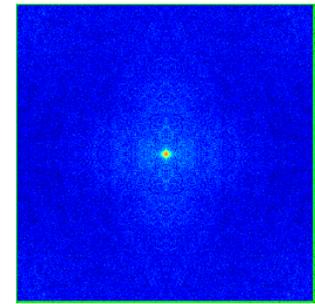
Spatial Correlation



Spatial correlation before subtracting background



Subtract the average



Spatial Correlation of entire image After subtracting image

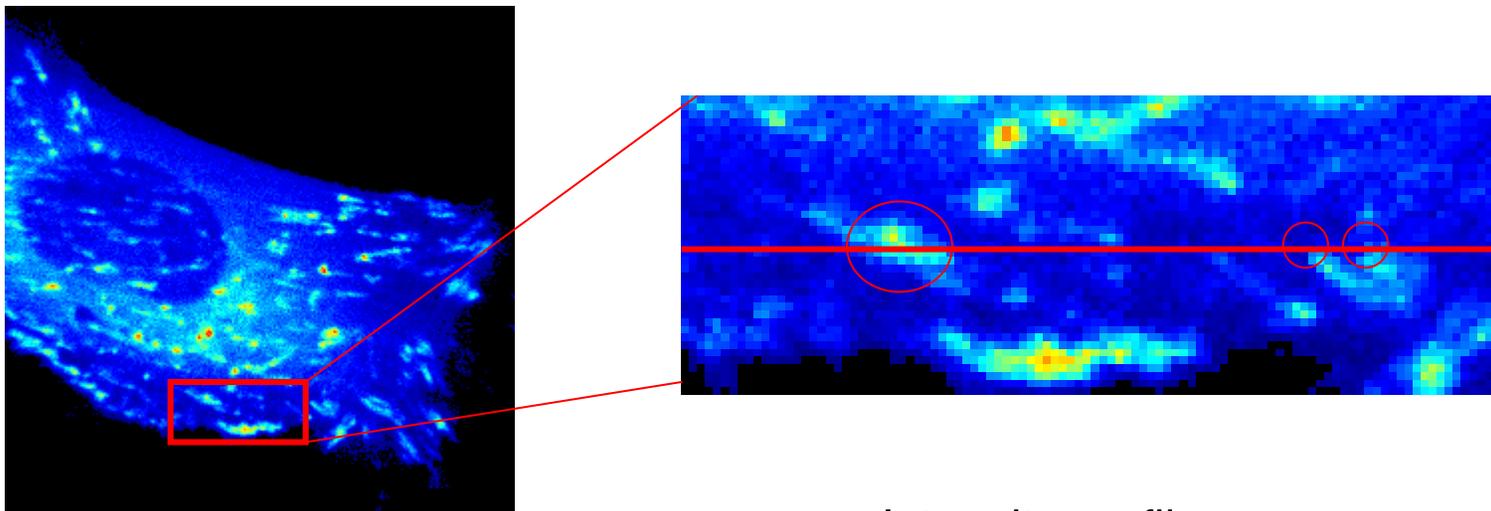
Average intensity of each pixel on the overall stack: $\overline{I(x, y)}$

$I_i(x, y) - \overline{I(x, y)}$ The intensity of each pixel minus the average intensity from entire stack for each pixel: However, this yields negative values.

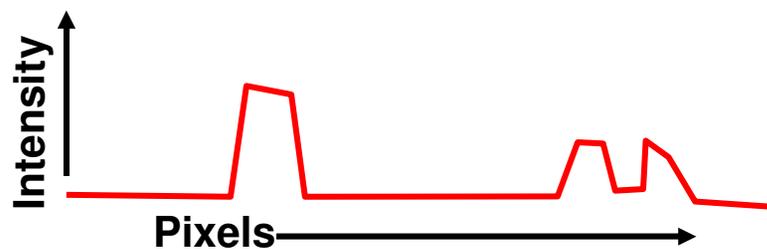
A scalar must be added : $a = \overline{I}$

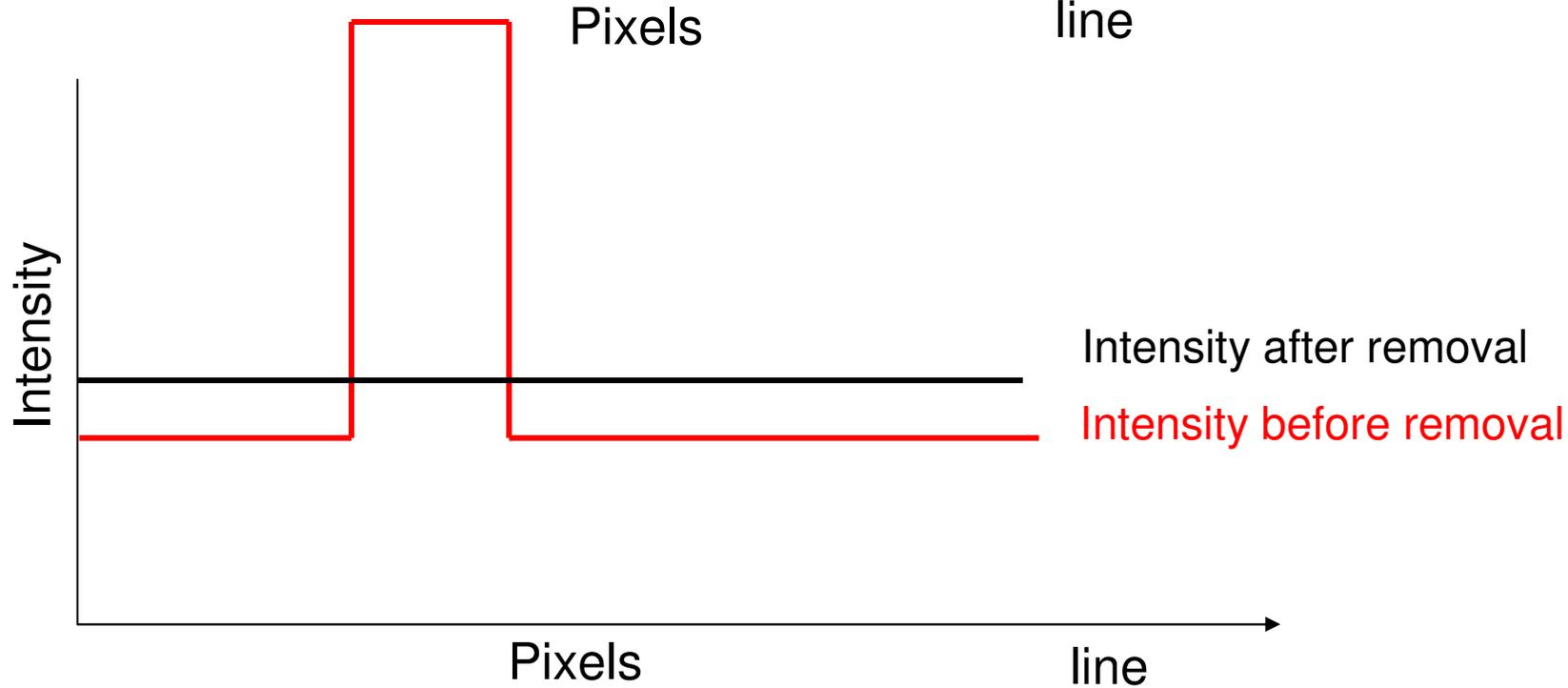
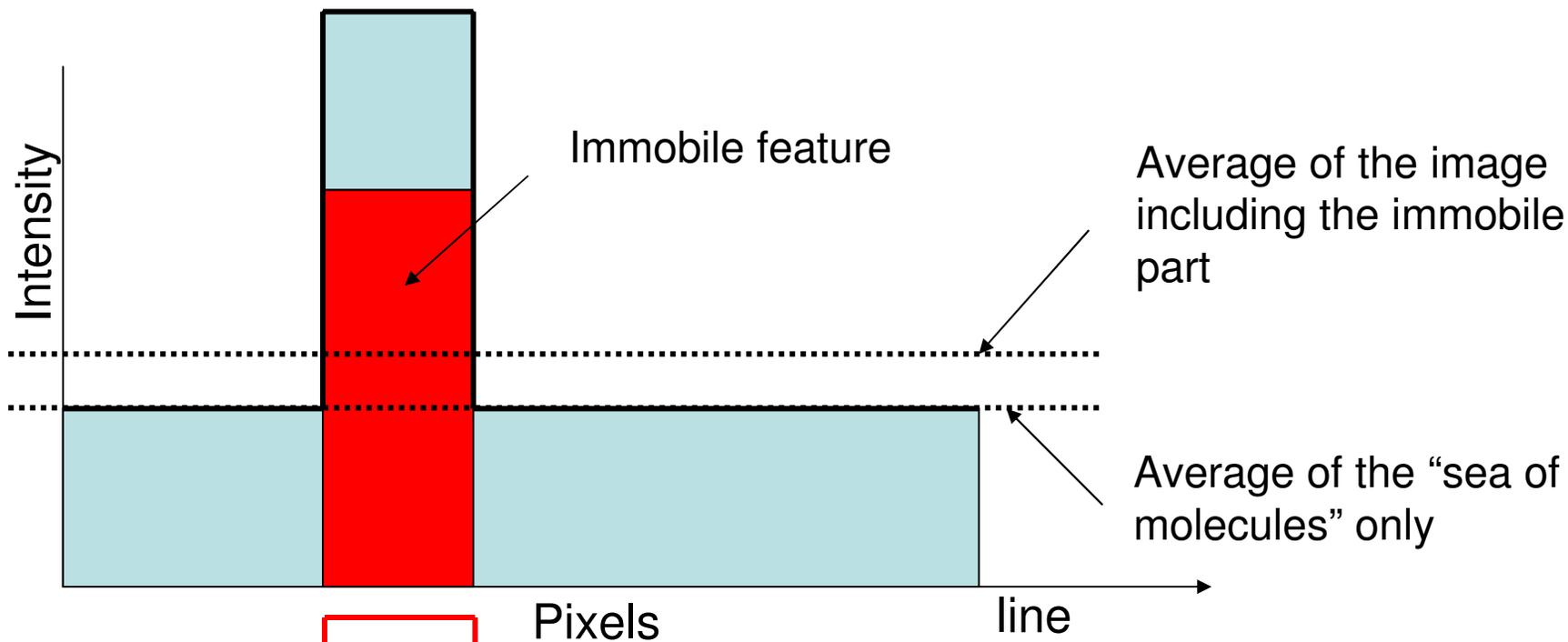
$$ICS(F_i(x, y)) \quad \text{where} \quad F_i(x, y) = I_i(x, y) - \overline{I(x, y)} + a$$

How to subtract immobile features from images?

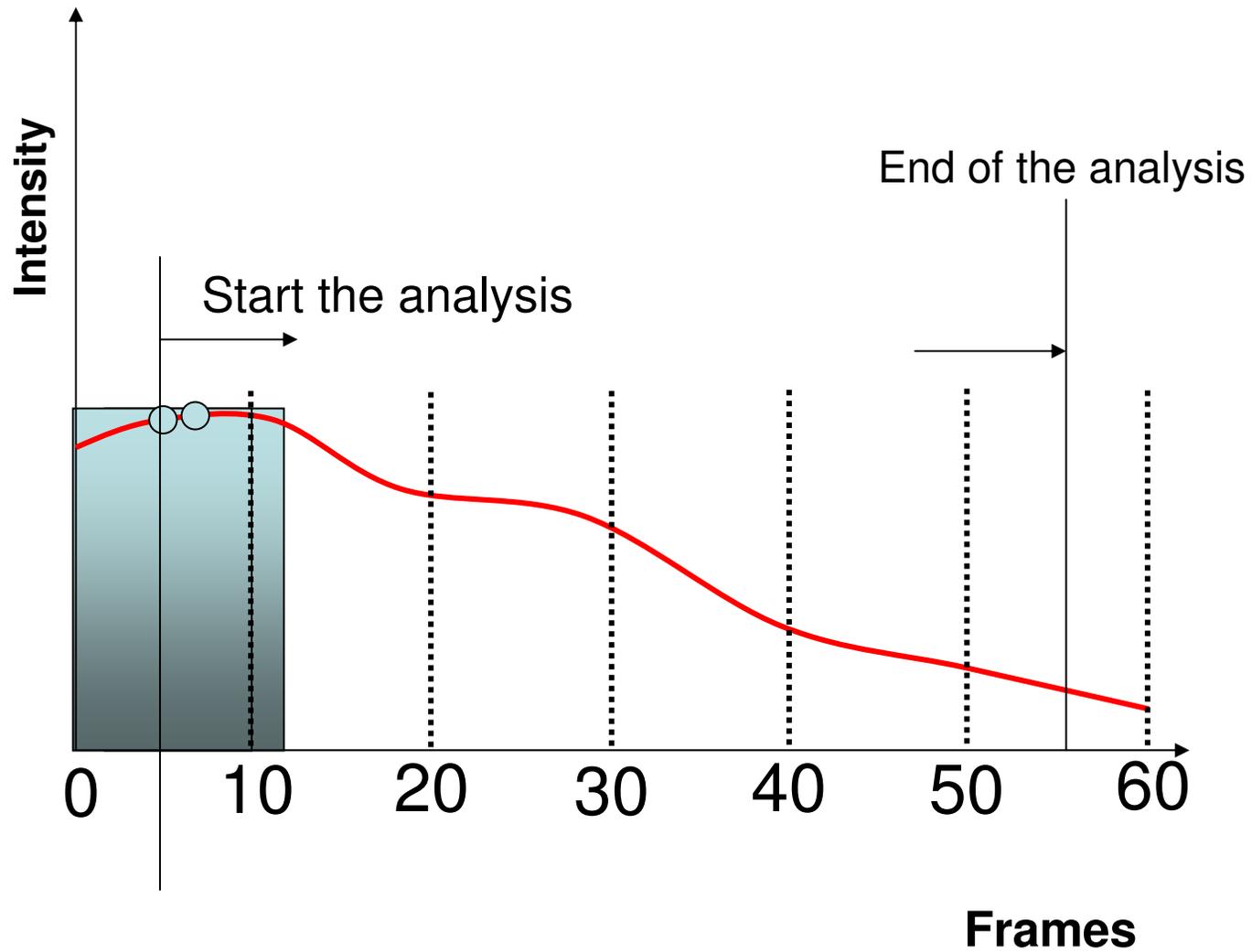


Intensity profile

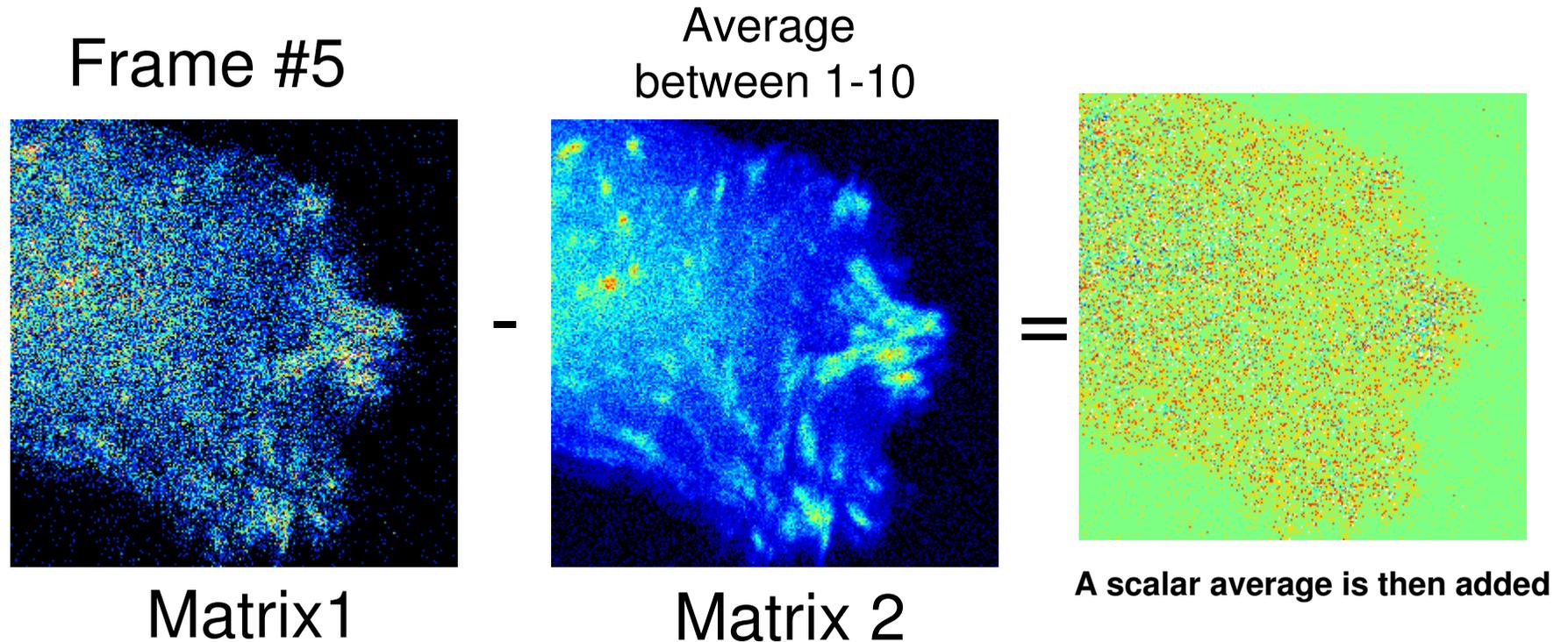




Subtraction of moving average

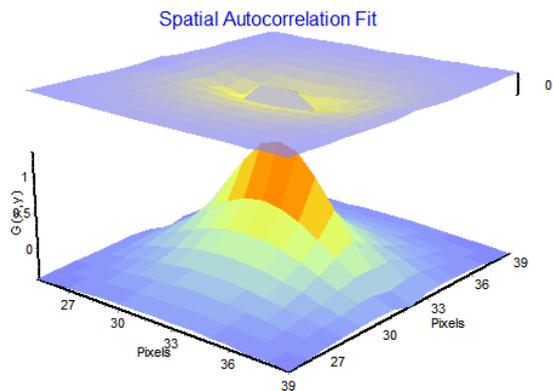
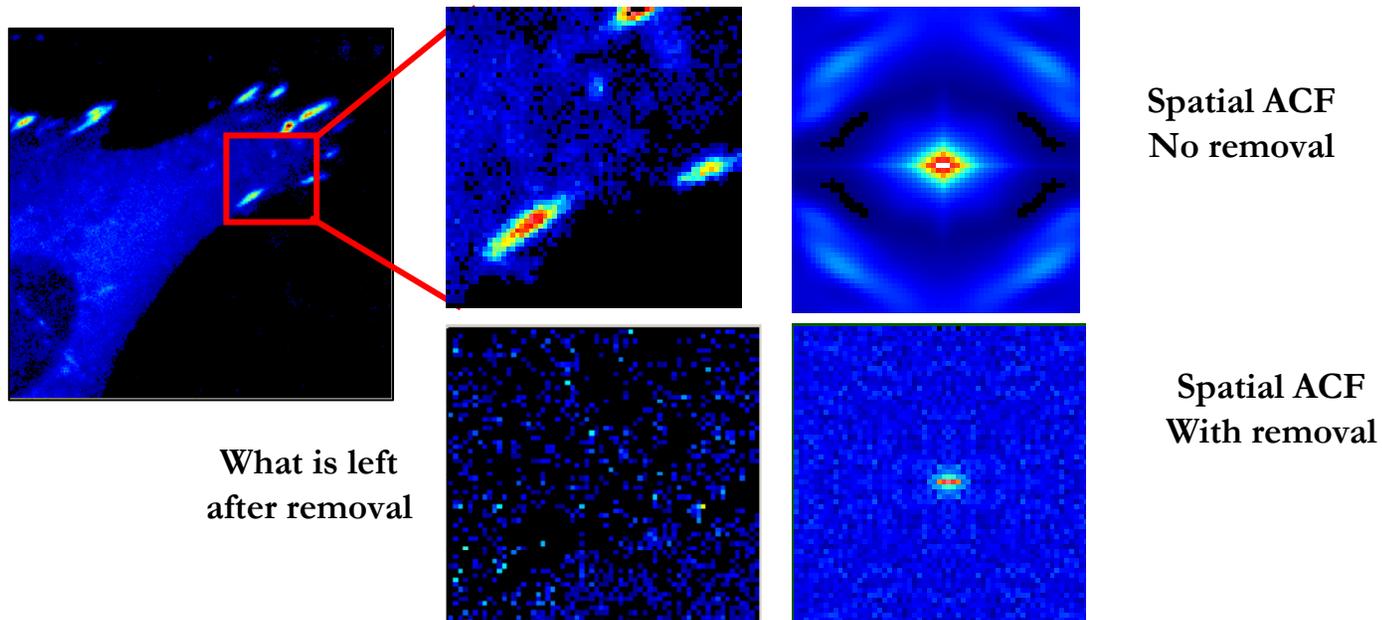


Moving average operation on frames:



Operation is repeated for frame #6 - average between 2-11
frame #7 - average between 3-12

Example of the Removal of Immobile Structures and Slow Moving Features



Fit using 3-D diffusion formula

Pixel size = $0.092\mu\text{m}$
 Pixel time = $8\mu\text{s}$
 Line time = 3.152ms
 W_0 = $0.35\mu\text{m}$

$$G1(0) = 0.0062$$

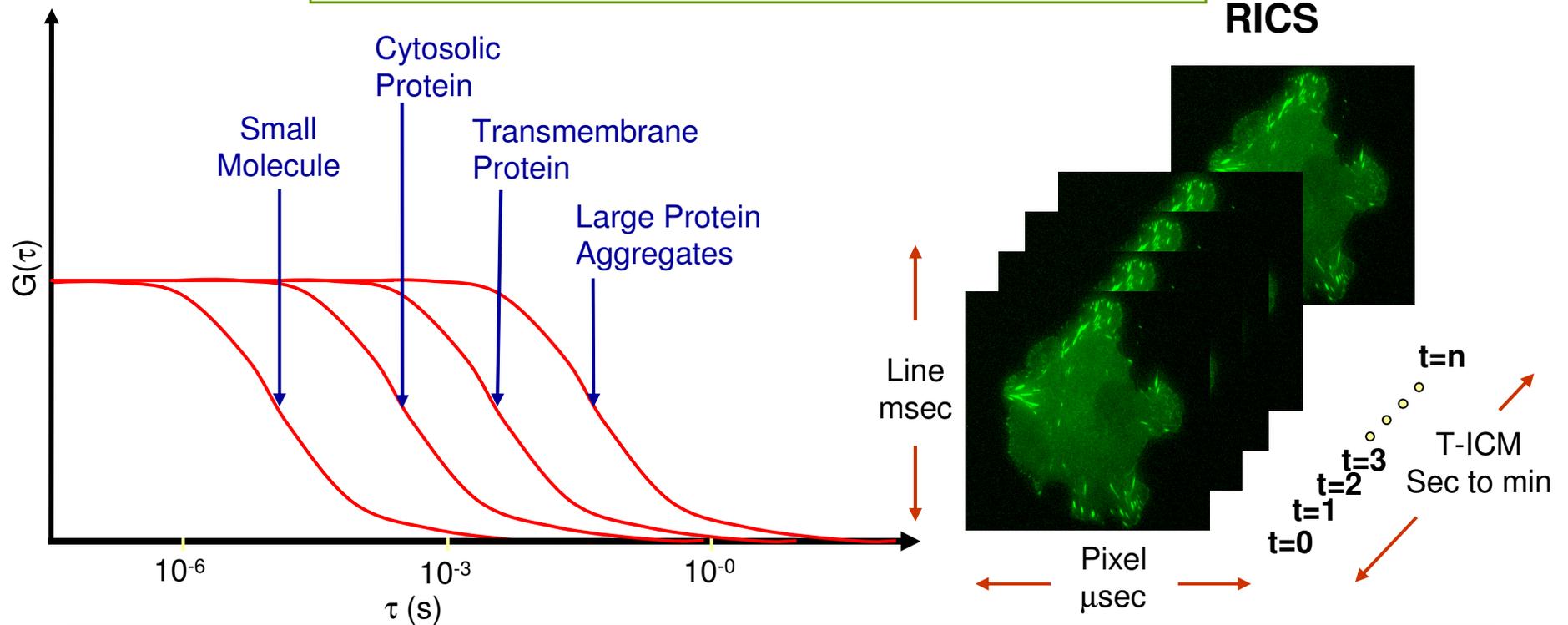
$$D1 = 7.4\mu\text{m}^2/\text{s}$$

$$G2(0) = 0.00023$$

$$D2 = 0.54\mu\text{m}^2/\text{s}$$

$$\text{Bkgd} = -0.00115$$

Conclusions



Techniques	Time Res.	Spatial Res.	Used to Study
FCS	sec	<0.5 μ m	Protein aggregates Transmembrane proteins
Temporal ICM	sec	<0.5 μ m	Protein aggregates Transmembrane proteins
RICS	μ sec-msec	~2 μ m	Soluble proteins Binding interactions
RICS	μ sec-msec	~2 μ m	Soluble proteins Binding interactions
Line-RICS	msec	<0.5 μ m	Soluble proteins Binding interactions

Summary

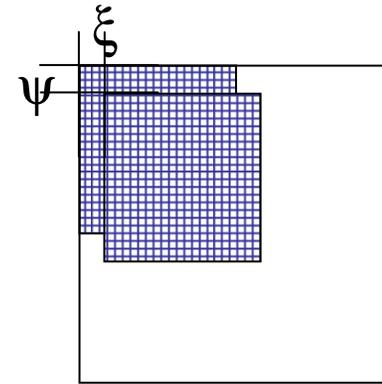
- **Measures dynamic rates from the μsec -msec time scale**
- **Anyone with a commercially available instrument can use it**
- **Immobile structures can be filtered out and fast fluctuations can be detected**
- **RICS has high spatial and temporal resolution**
- **The range of these dynamic rates covers a wide range from immobile to cytosolic diffusions (0.2-12 $\mu\text{m}^2/\text{s}$)**
- **Other types of processes and interactions are also measured**
- **Line scanning is essential for determination of binding process and complements the RICS analysis**

We have expanded the RICS
methods to do Cross-Correlation
RICS (ccRICS)

The ccRICS approach

The spatial correlation function

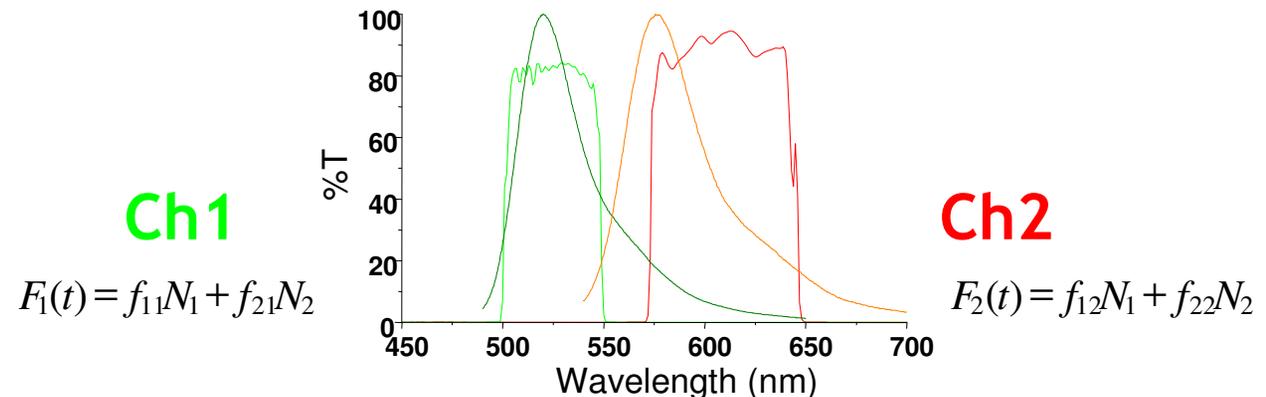
$$G_{ccRICS}(\xi, \psi) = \frac{\langle I_1(x, y) I_2(x + \xi, y + \psi) \rangle}{\langle I_1(x, y) \rangle \langle I_2(x, y) \rangle} - 1$$



The variables ξ and ψ represent spatial increments in the x and y directions, respectively

The $G_{cc}(0,0)$ value and bleedthrough

$$G_{cc}(0,0) \propto \left[\frac{f_{11} f_{12} \langle N_1 \rangle + f_{21} f_{22} \langle N_2 \rangle}{f_{11} f_{12} \langle N_1 \rangle^2 + (f_{11} f_{22} + f_{21} f_{12}) \langle N_1 \rangle \langle N_2 \rangle + f_{21} f_{22} \langle N_2 \rangle^2} \right]$$



Experimental issues

- The volume of excitation and emission at the two excitation wavelengths must superimpose (we are using the Olympus FV1000 LSCM for these experiments)
- Bleedthrough of the green into the red channel must be small (<5%)
- FRET will strongly decrease the ccRICS signal
- High ratio of labeled to unlabeled molecules are needed (if you have only 10% labeled, in a complex of 1:1, you will only have 1% of the complexes labeled with both proteins)

Cells. MEF transfected Vinculin, FAK and paxillin. cDNA were ligated to EGFP or mCherry at the C-terminal end.

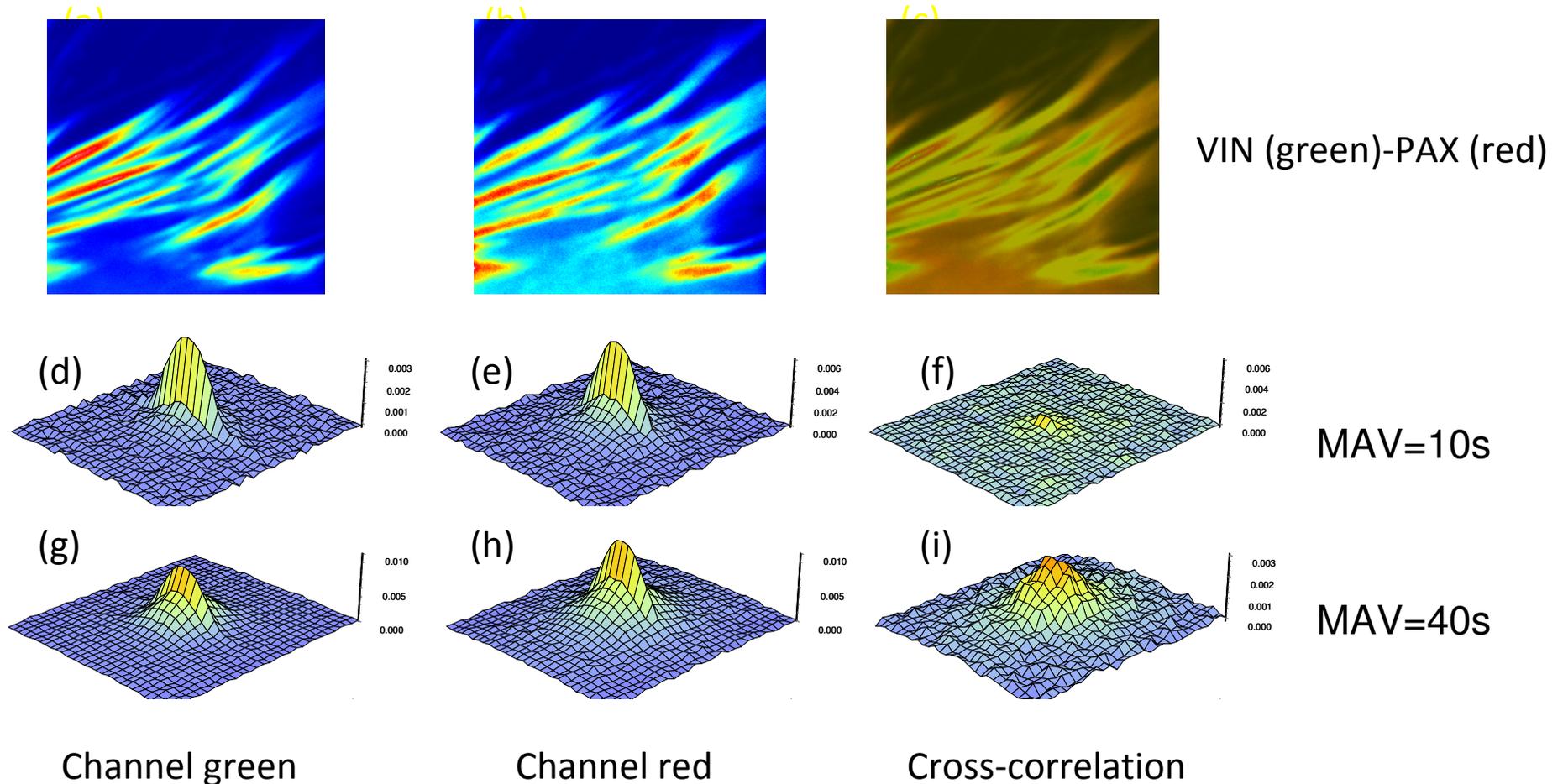
Microscopy. Olympus FV1000 with 60x 1.2NA water objective, 12.5 us/pixel, 256x256 pixels 12.5 μm square, 100 to 200 frames collected for each sample. 1frame/s.

EGFP excitation at 488nm (0.5%) and mCherry at 559nm (adjusted to a max of 1.5%).

Emission filters at 505-540nm and 575-675 nm, for the green and red channels, respectively.

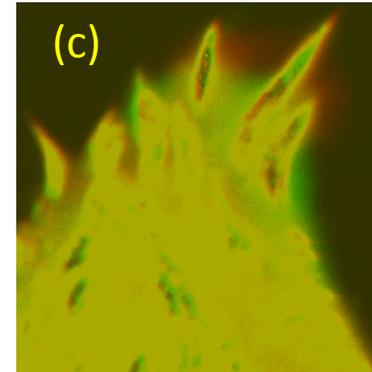
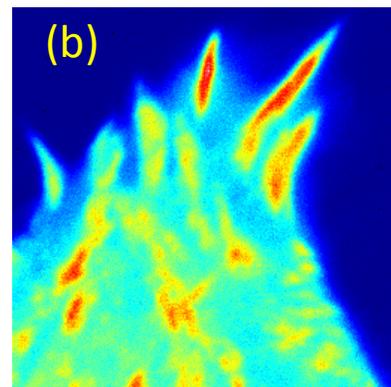
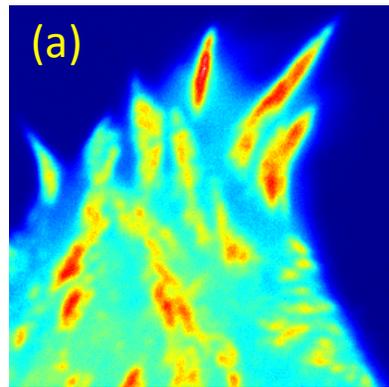
Overlap of the volume of observation was tested by imaging single 100 nm fluorescent beads carrying two colors simultaneously

VIN and PAX co localize at adhesions but they are moving independently in the cytoplasm

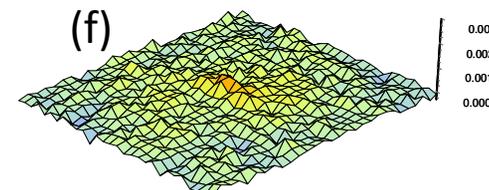
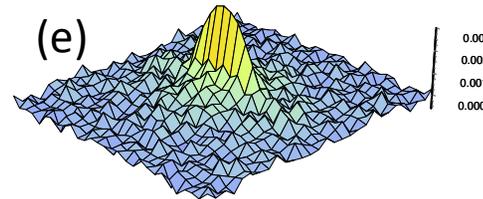
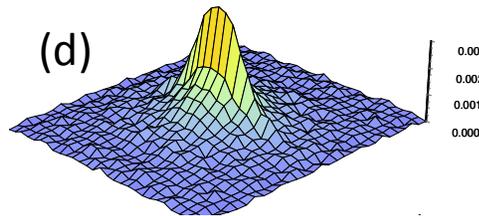


The cross-correlation increases for the slow fluctuations (at MAV=40s). It is round in shape indicating that it is generated at single locations.

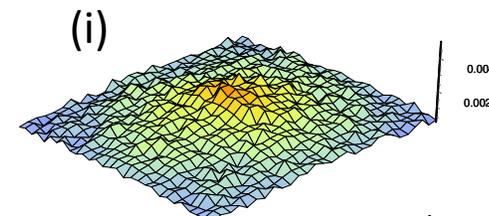
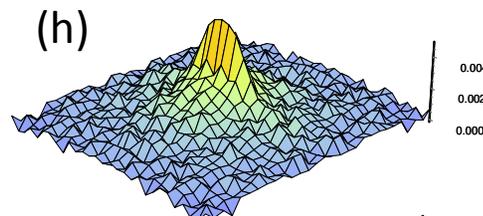
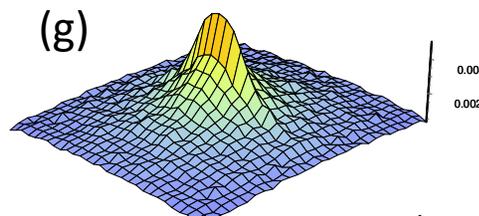
FAK and PAX co localize at adhesions but they are moving independently in the cytoplasm



FAK (green)-PAX (red)



MAV=10s



MAV=40s

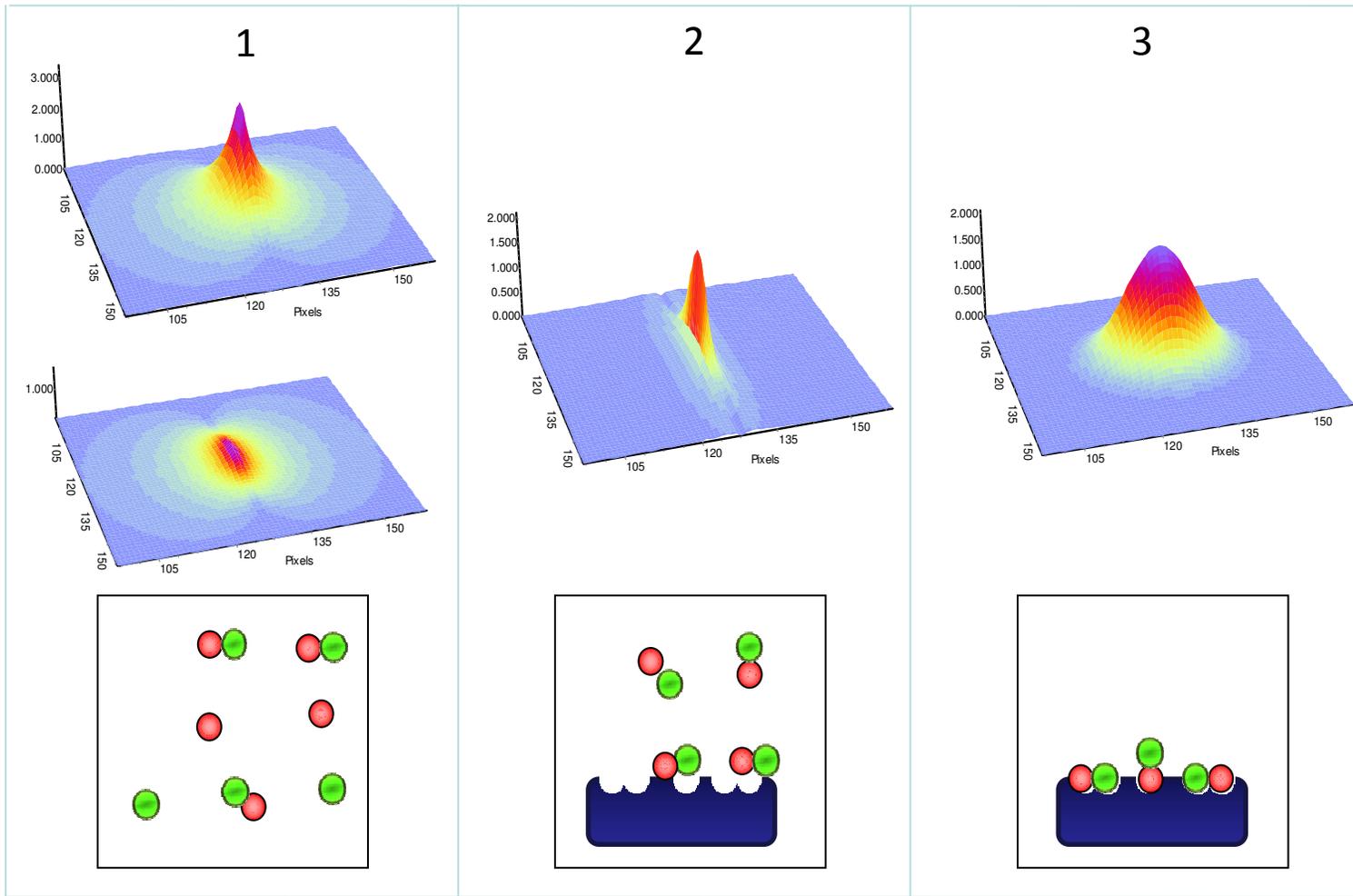
Channel green

Channel red

Cross-correlation

The cross-correlation increases for the slow fluctuations (at MAV=40s). It is round in shape indicating that it is generated at single locations and it is very small.

Schematic representation for the interpretation of the ccRICS experiment. Simulation of binding and diffusion

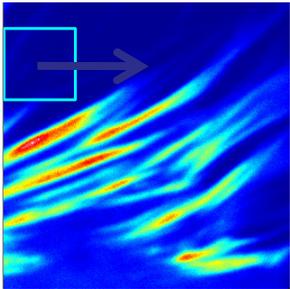


Diffusion
Few complexes

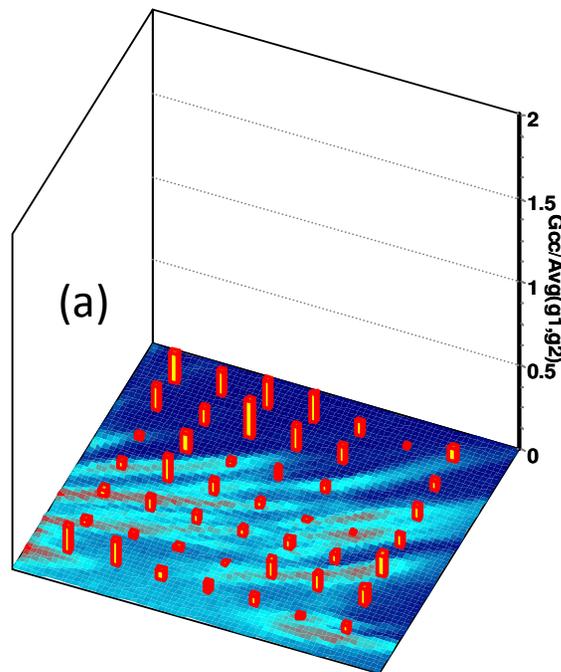
Fast binding
Different shape
Smaller than PSF

Slow binding
Round shape

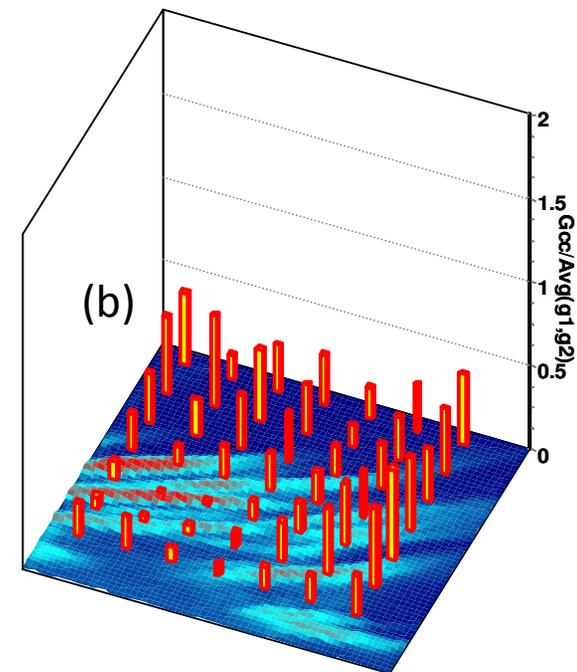
Distribution of fraction of cross-correlation in the cell. Correlation with adhesion disassembling



ccRICS by scanning a region of interest across the image
Calculating the ratio $G_{cc}/AV(G_1, G_2)$



VIN-PAX MAV=10s



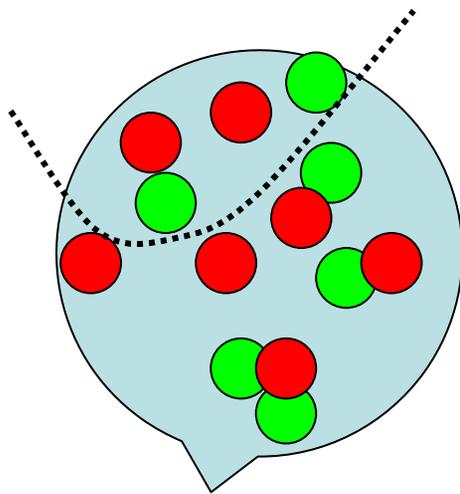
VIN-PAX MAV=40s

There is “more” cross-correlation at the locations of adhesion disassembling

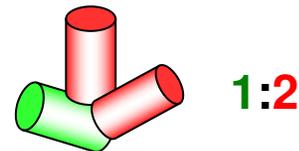
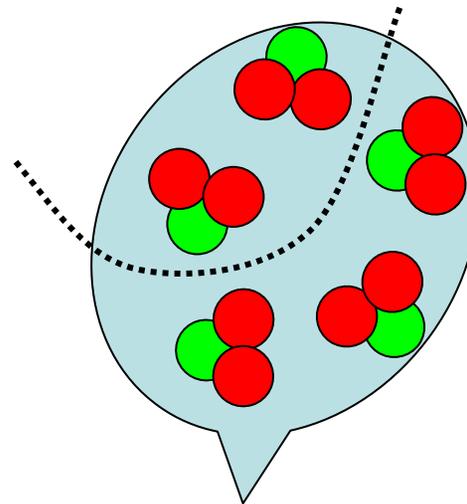
Summary of ccRICS

- We developed a **toolbox** for biophysicists and cell biologists to address common questions regarding the formation of protein complex, their spatial distribution and their stoichiometry
- **ccRICS** is extremely powerful at detecting joint diffusing proteins and in separating diffusion from binding processes
- The Paxillin, vinculin and FAK never crosscorrelate in the cytoplasm before binding to the focal adhesion. We only detect cross correlation due to dissociation of large clusters of proteins.

What is the stoichiometry of these clusters
and is this stoichiometry crucial for the
biological system?



Random



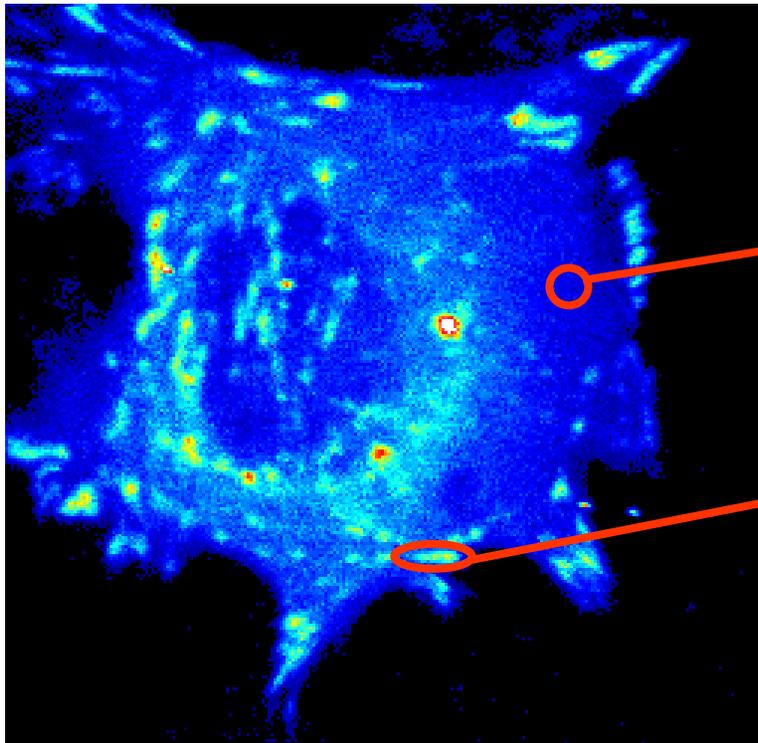
The Number & Molecular Brightness (N&B) Method

UCIrvine
UNIVERSITY OF CALIFORNIA, IRVINE



Existing Methods to determine protein concentration and aggregation of proteins in cells

1. Calibration of the free fluorophore based on intensity



Average intensity of MEF cells expressing Paxillin-EGFP

A INTENSITY
31,250 counts/sec

B
93,750 counts/sec

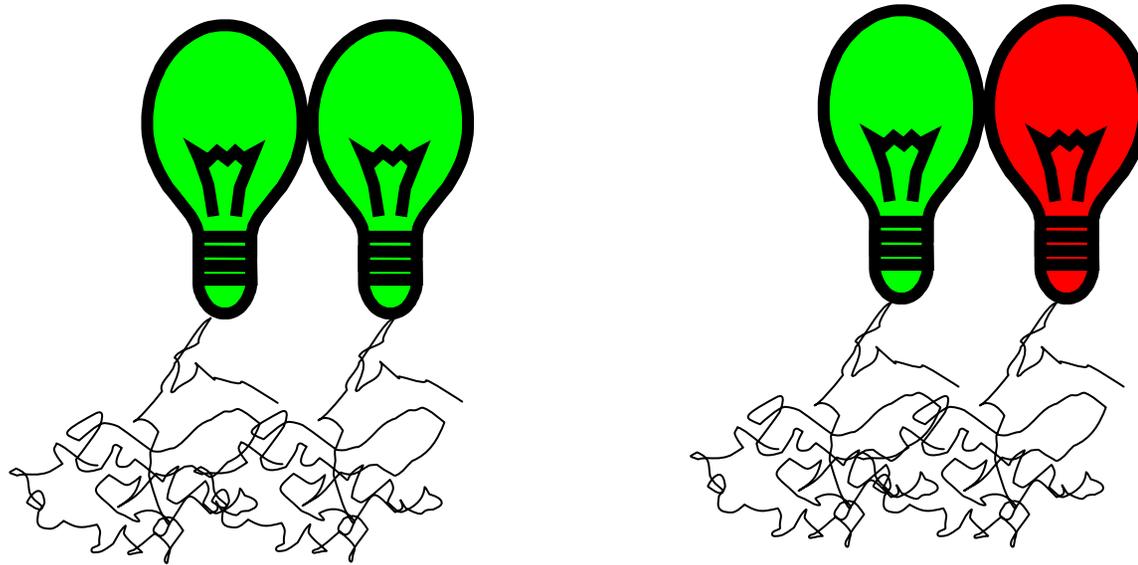
If “free” EGFP at 10nM gave 30,000 counts/sec then the conclusion would be that :

A = 10nM

B = 30nM

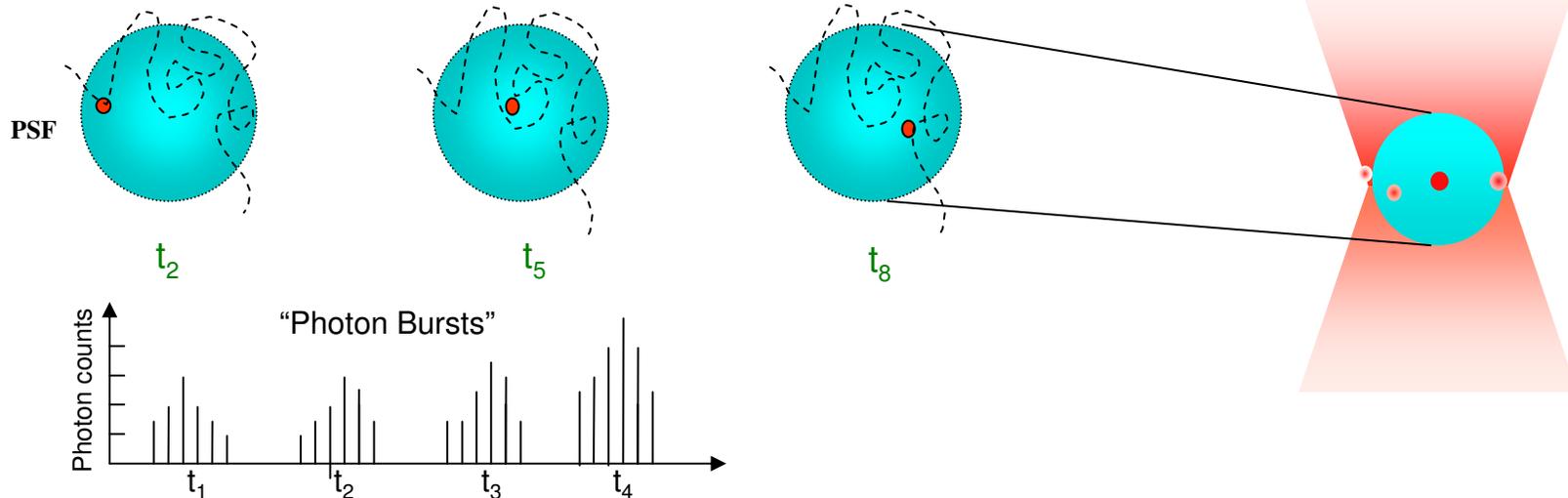
**However, it doesn't give you the size distribution
Only concentration is given**

2. Förster resonance energy transfer (FRET)

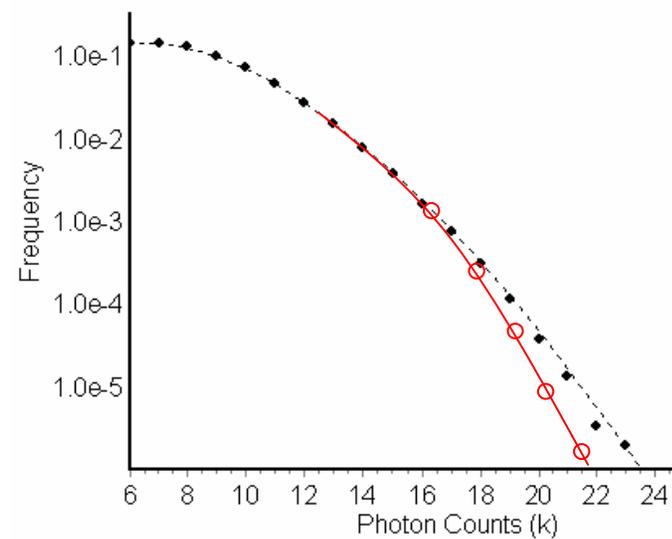
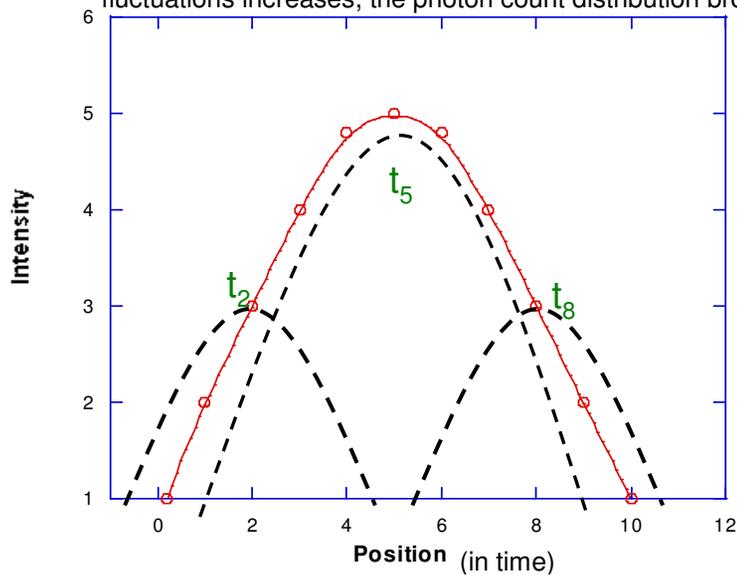


This method is very sensitive to detect the formation of pairs.

THE AVERAGE PHOTON COUNT RATE OF BURSTS DETERMINES THE MOLECULAR BRIGHTNESS OF THE LABELED PROTEIN.

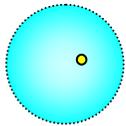


The intensity distribution accounts for the fluctuations of photons from the molecule freely diffusing through the excitation profile. Thus, the overall photon counting count distribution is the weighted superposition of individual Poissonian distributions for each intensity values with a scaling amplitude. The fluctuations light intensity results in a broadening of photon count distribution with respect to a pure poisson distribution. As the fluctuations increases, the photon count distribution broadens.

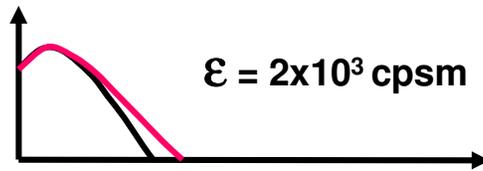


4. Photon Counting Histogram Analysis

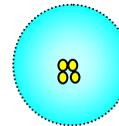
Many particles one brightness



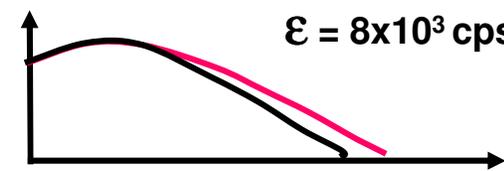
Single paxillin



One particle increasing brightness

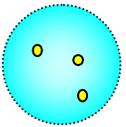


cluster of 4 paxillins

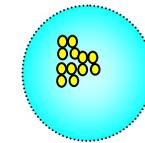
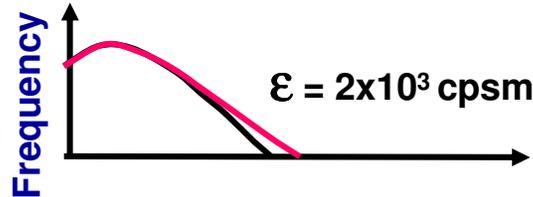


Significant difference

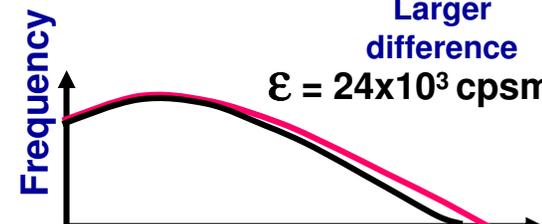
$\epsilon = 8 \times 10^3$ cpsm



Few paxillin
Not aggregated

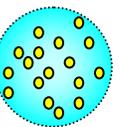


large paxillin
self-aggregate

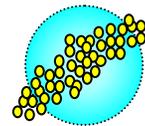
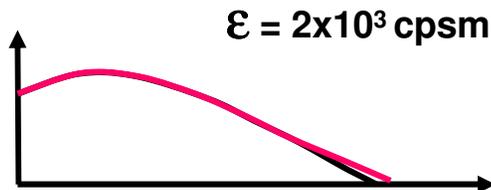


Larger difference

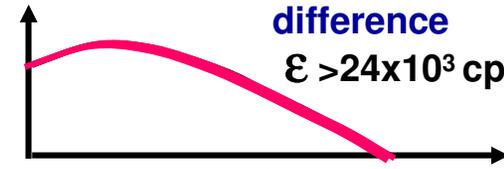
$\epsilon = 24 \times 10^3$ cpsm



Many paxillin
Not aggregated



large cluster

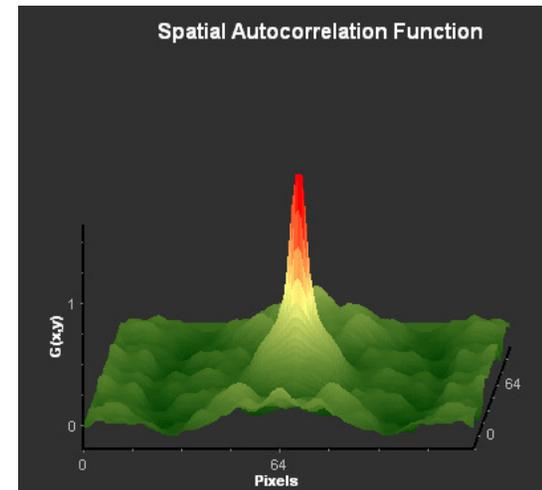
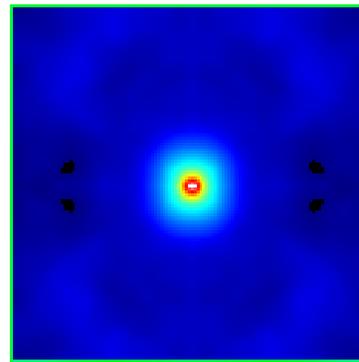
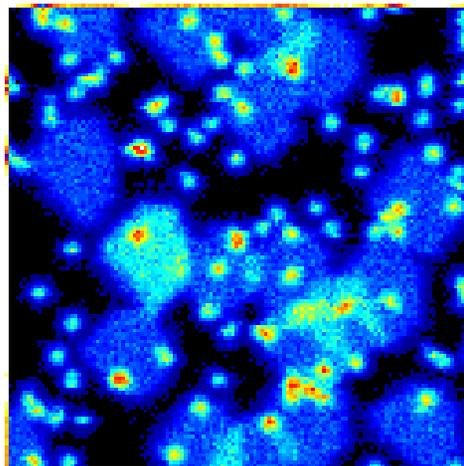
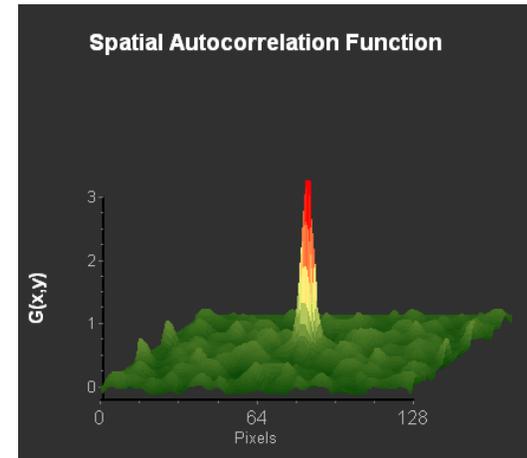
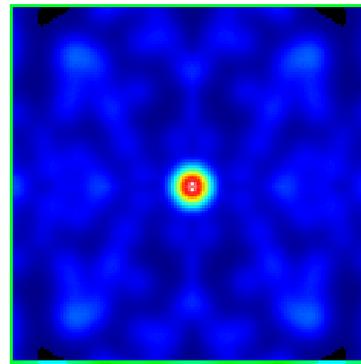
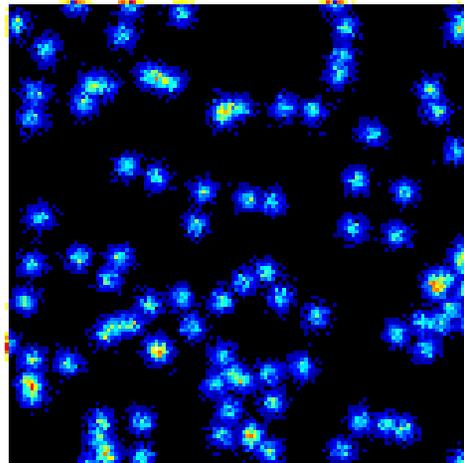


No difference

$\epsilon > 24 \times 10^3$ cpsm

Red is PCH
Black is Poisson

3. Image correlation Spectroscopy (ICS)



However, the events must be slow >1 sec (no movement during one frame) and the aggregates must be large.

Petersen and Wiseman:Biophys J. 1999

The Number and Brightness (N&B) analysis

Purpose: Provide a pixel resolution map of molecular number and aggregation in cells

Method: First and second moment of the fluorescence intensity distribution at each pixel

Source: Raster scanned image obtained with laser scanning microscopes
TIRF with fast cameras
Spinning disk confocal microscope

Output: The N and B maps, B vs intensity 2D histogram

Tools: Cursor selection of pixel with similar brightness
Quantitative analysis of center and std dev of the e and n distribution
Tools for calibration of analog detectors

Tutorials: mathematical background, data import, analysis examples (our web site)

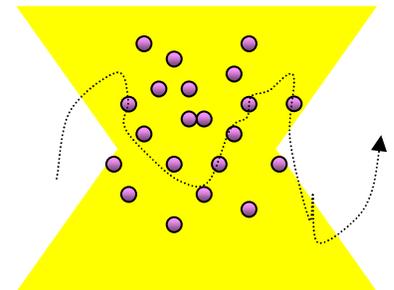
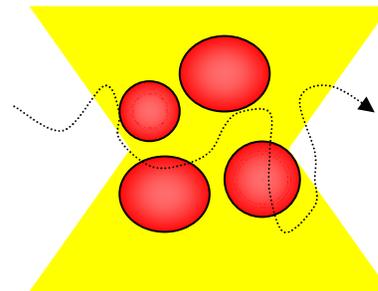
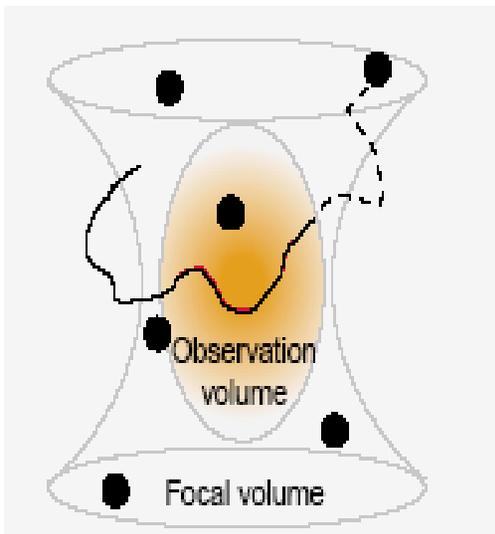
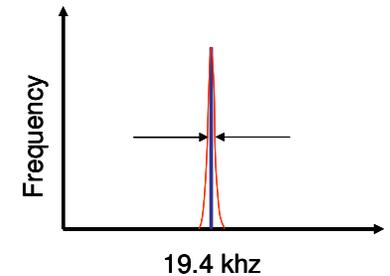
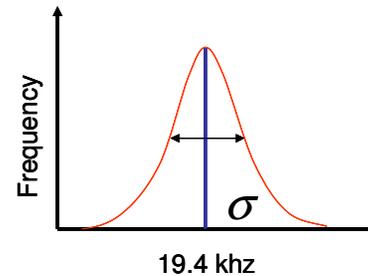
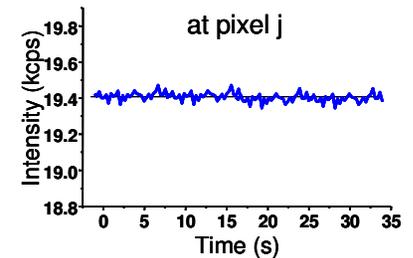
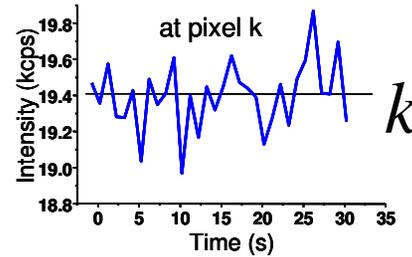
How to distinguish pixels with many dim molecules from pixels with few bright molecules?

**Average
(first moment)**

$$\langle k \rangle = \frac{\sum_i k_i}{K}$$

**Variance
(second moment)**

$$\sigma^2 = \frac{\sum_i (k_i - \langle k \rangle)^2}{K}$$



- Given two series of equal average, the larger is the variance, the less molecules contribute to the average. The ratio of the square of the average intensity ($\langle k \rangle^2$) to the variance (σ^2) is proportional to the average number of particles $\langle N \rangle$.

$$G(0) = \sigma^2 / \langle k \rangle^2 = 1/N$$

* Originally developed by Qian and Elson (1990) for solution measurements.

Calculating protein aggregates from images

This analysis provides a map of $\langle N \rangle$ and brightness (B) for every pixel in the image. The units of brightness are related to the pixel dwell time and they are “counts/dwell time/molecule”.

$$\langle k \rangle = \frac{\sum_i k_i}{K} \quad \sigma^2 = \frac{\sum_i (k_i - \langle k \rangle)^2}{K}$$

$$B = \frac{\langle k \rangle}{\langle N \rangle} = \frac{\sigma^2}{\langle k \rangle}$$

$$\langle N \rangle = \frac{\langle k \rangle^2}{\sigma^2}$$

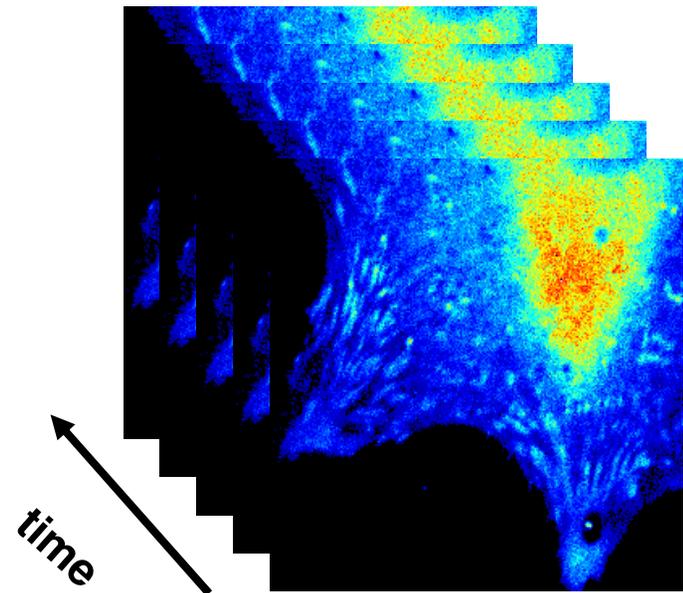
σ^2 = Variance

$\langle k \rangle$ = Average counts

N = Apparent number of molecules

B = Apparent molecular brightness

K = # of frames analyzed



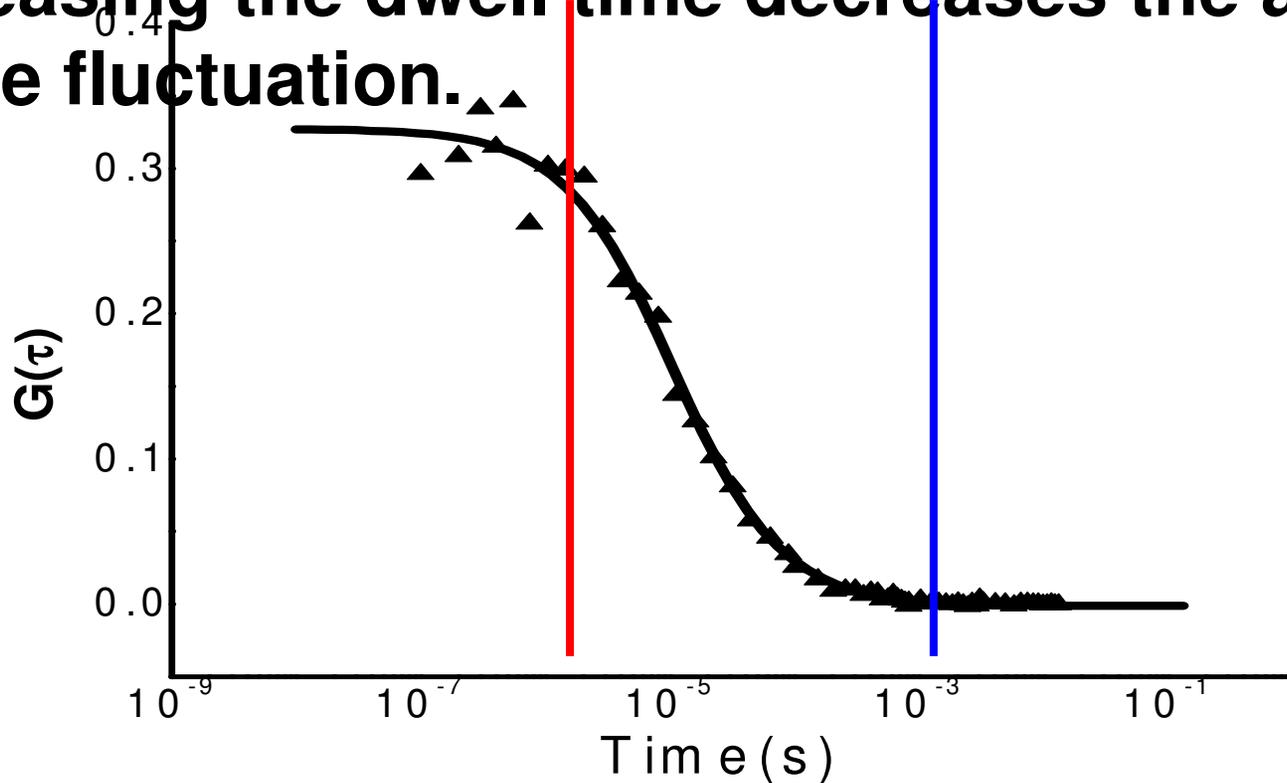
Selecting the dwell time

To increase the apparent brightness we could increase the dwell time, since the brightness is measured in counts/dwell time/molecule.

1 μ s dwell time

1 ms dwell time

Increasing the dwell time decreases the amplitude of the fluctuation.



What contributes to the variance?

Variance due to particle number fluctuations

$$\sigma_n^2 = \varepsilon^2 n$$

Variance due to detector shot noise

$$\sigma_d^2 = \varepsilon n$$

The measured variance contains two terms, the variance due to the particle number fluctuation and the variance due to the detector count

These two terms have different dependence on the

$$\sigma_n^2 = \varepsilon^2 n$$

$$\sigma_d^2 = \varepsilon n$$

(for the photon counting detector)

Both depend on the intrinsic brightness and the number of molecules. We can invert the equations and obtain n and ε

n is the true number of molecules
 ε is the true molecular brightness

How to Calculate n and ε

$$B = \frac{\sigma^2}{\langle k \rangle} = \frac{\sigma_n^2}{\langle k \rangle} + \frac{\sigma_d^2}{\langle k \rangle} = \frac{\varepsilon^2 n}{\varepsilon n} + \frac{\sigma_d^2}{\langle k \rangle} = \varepsilon + 1$$

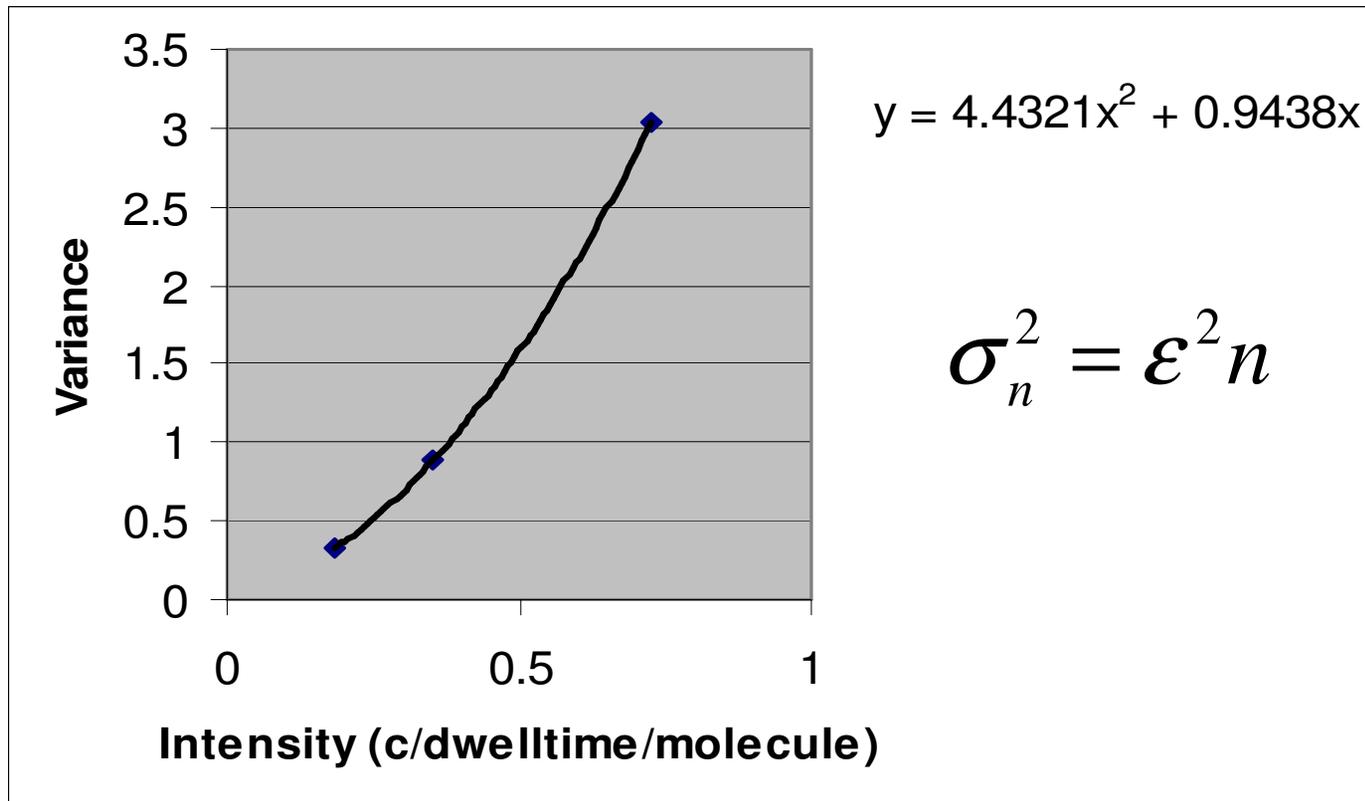
This ratio identifies pixels of different brightness due to mobile particles.

The “true” number of molecules n and the “true” molecular brightness for mobile particles can be obtained from

$$n = \frac{\langle k \rangle^2}{\sigma^2 - \langle k \rangle} \quad \varepsilon = \frac{\sigma^2 - \langle k \rangle}{\langle k \rangle}$$

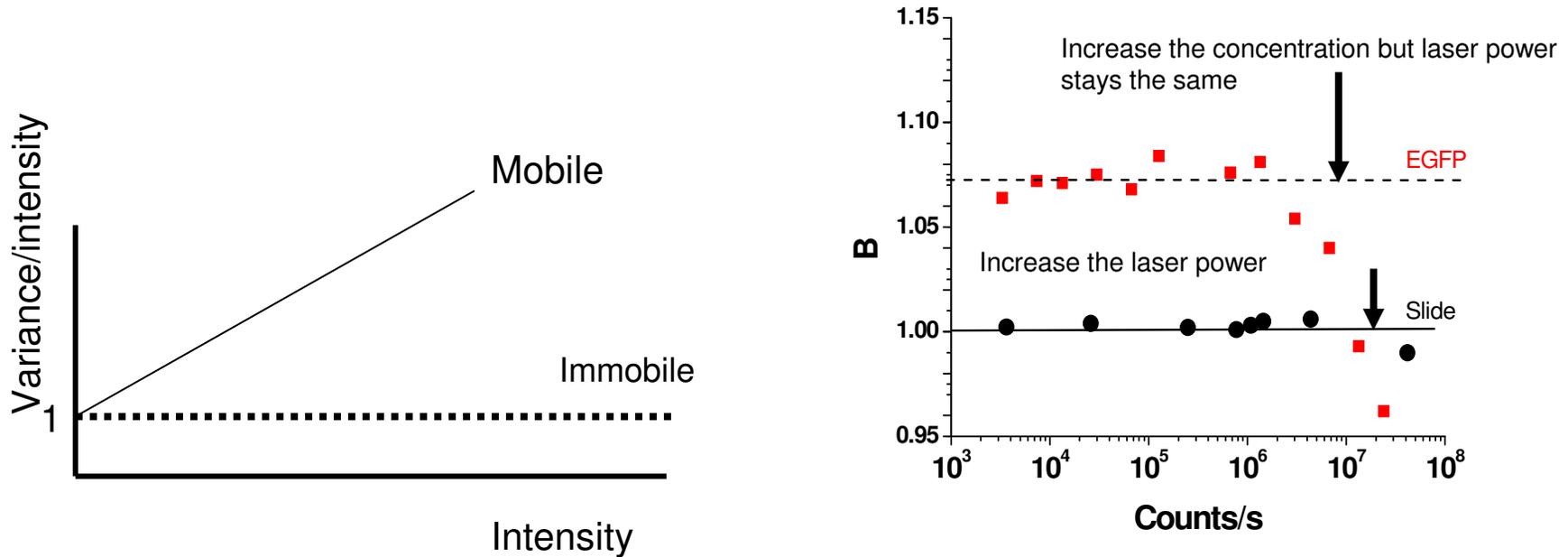
If there are regions of immobile particles, n cannot be calculated because for the immobile fraction the variance is = $\langle k \rangle$. For this reason, several plots are offered to help the operator to identify regions of mobile and immobile particles. Particularly useful is the plot of N vs B.

Quadratic dependence of the variance on particle brightness 20nM EGFP in solution as a function of laser power



2-photon excitation using photon counting det

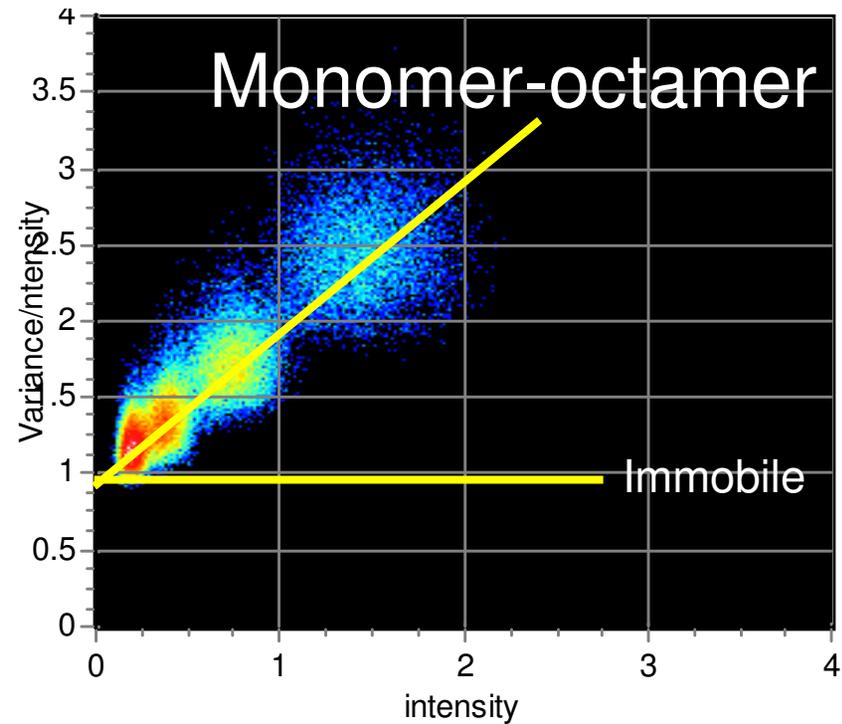
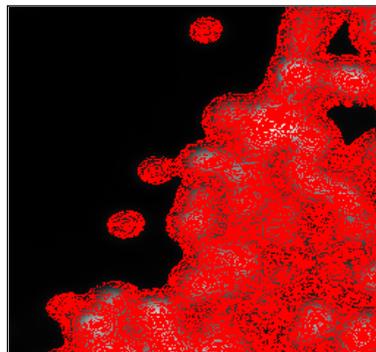
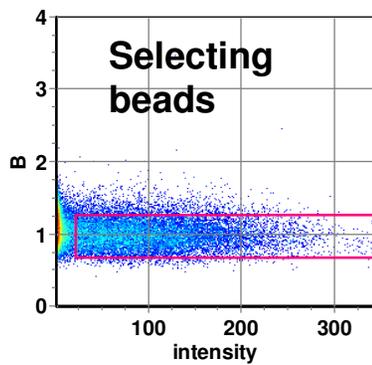
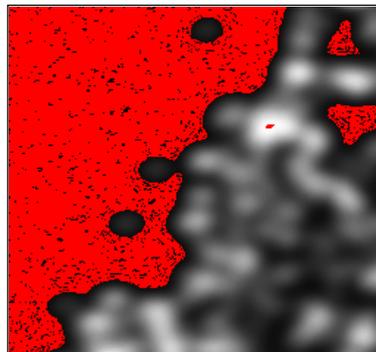
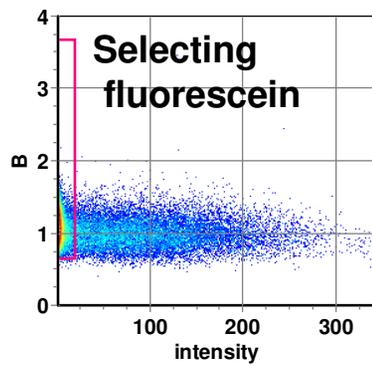
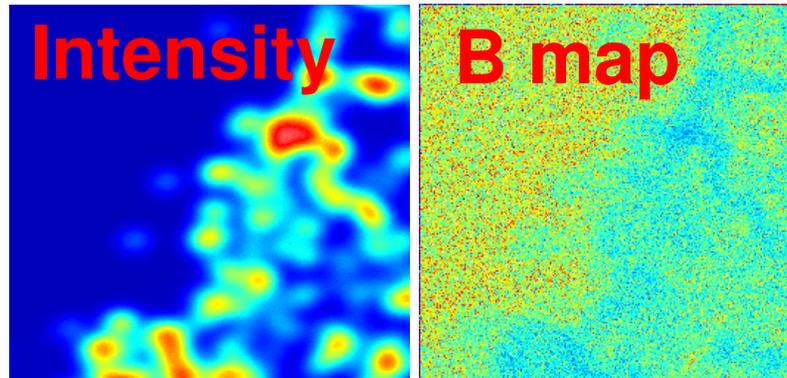
Identification of mobile and immobile molecules



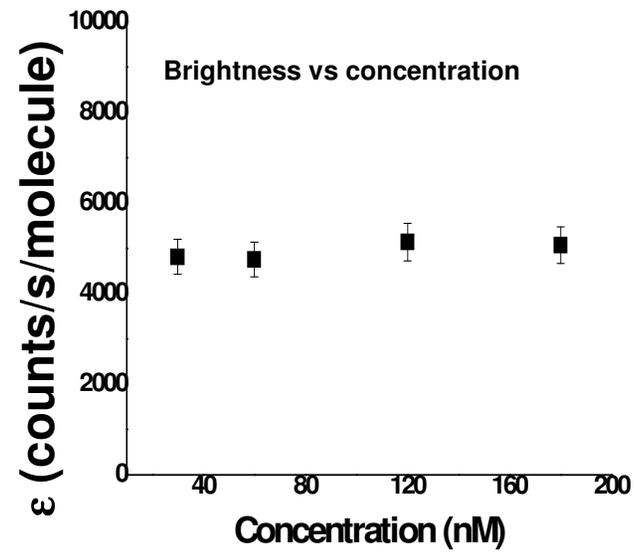
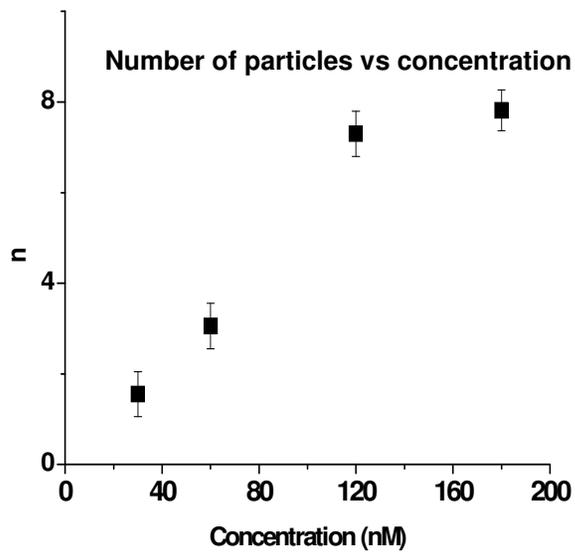
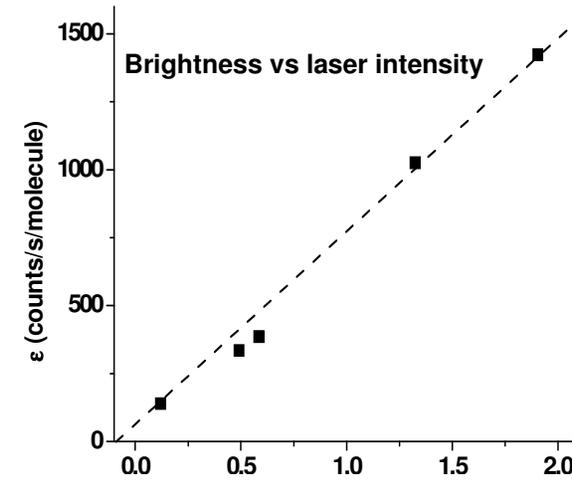
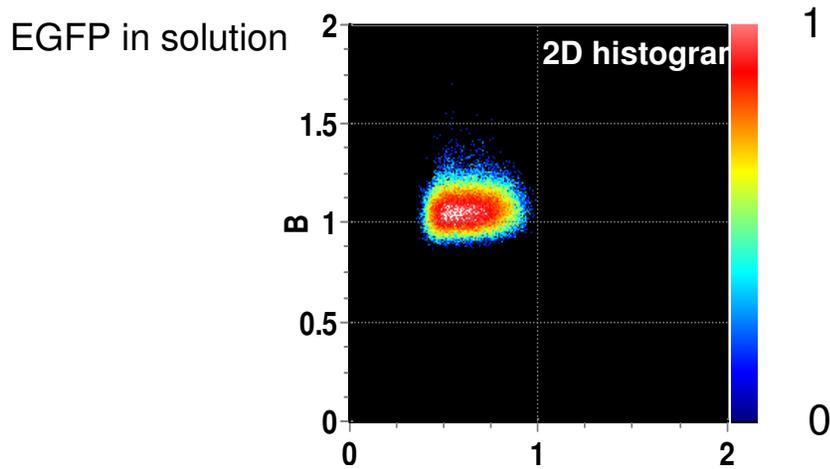
If we change the laser power, a plot of the ratio variance/intensity vs intensity can distinguish the mobile from immobile fraction. The two curves are for different pixel integration times.

The effect of the immobile part: with photon counting detectors

Fluorescent beads in a sea of 100nM Fluorescein.

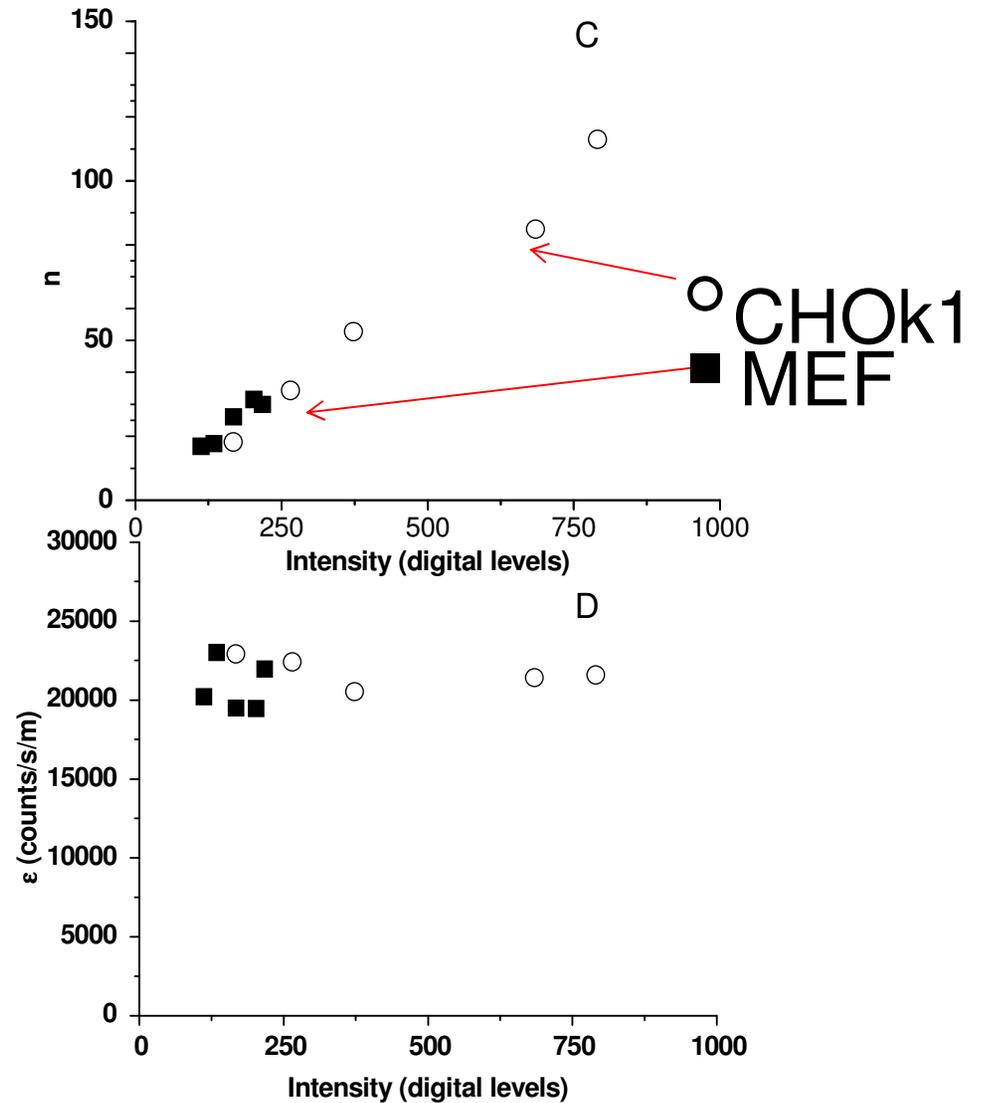
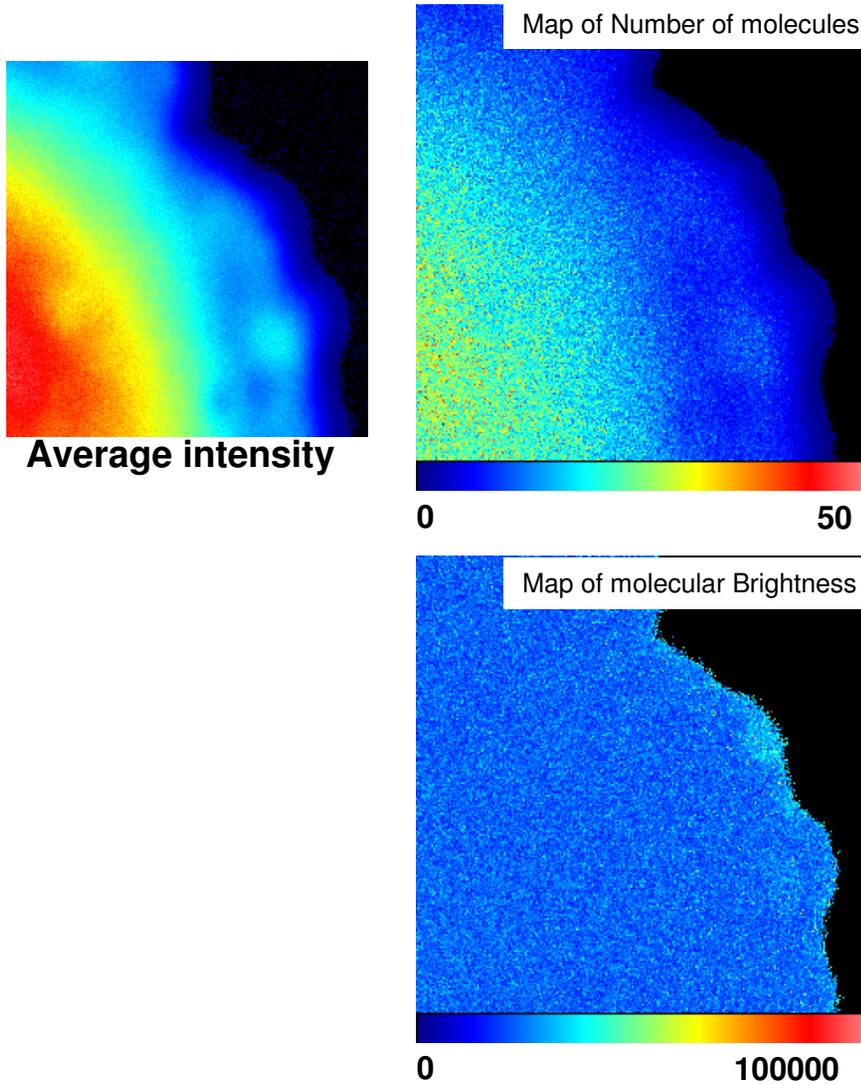


Brightness and number of molecules can be measured independently



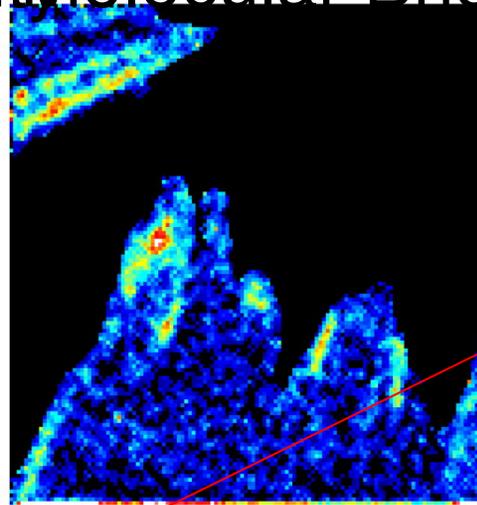
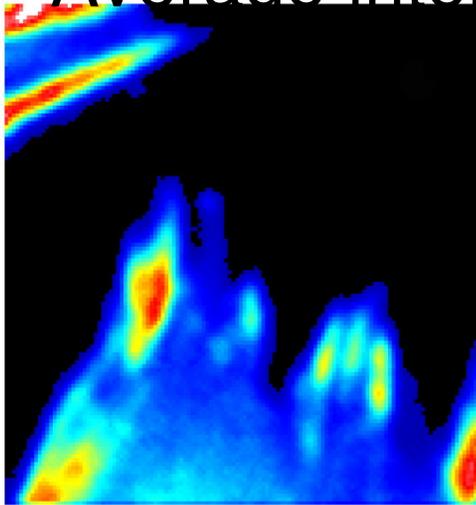
EGFP in CHO-k1 (1-Photon LSM)

homogenous Brightness & heterogeneous Number of Molecules

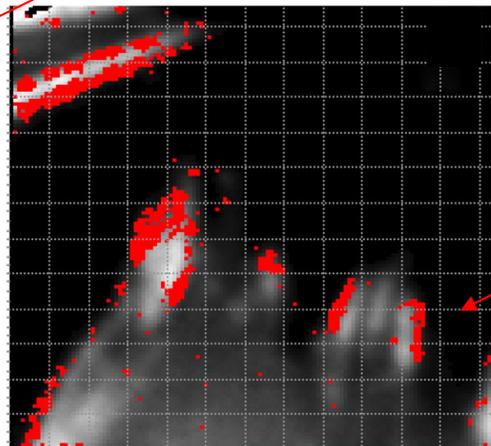
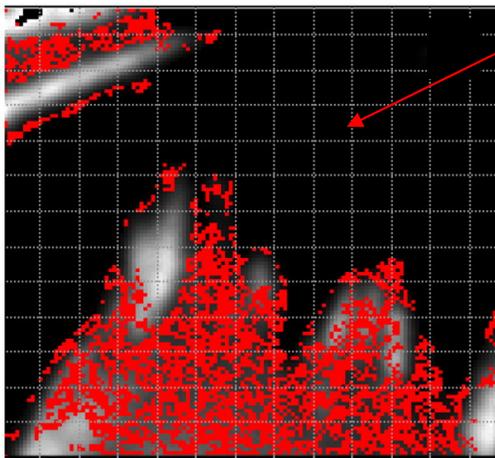
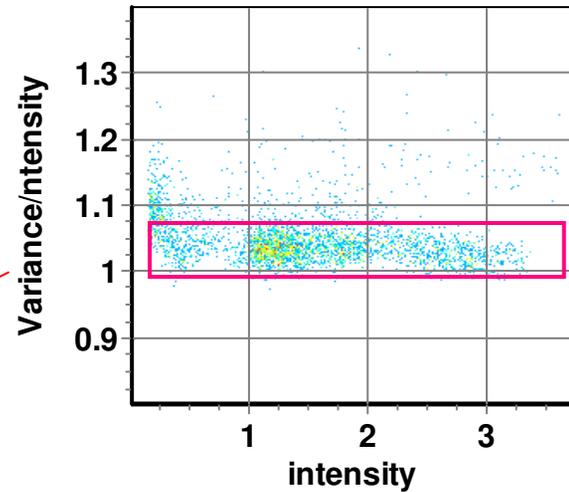


Paxillin assembles as monomers and disassembles as aggregates as large as 8-12

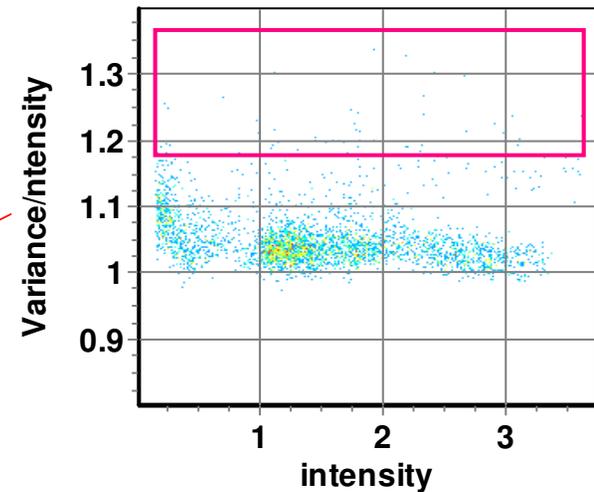
Average intensity Molecular Brightness



x= 1.90057 y= 1.03400 #pixels= 5702 in= 662



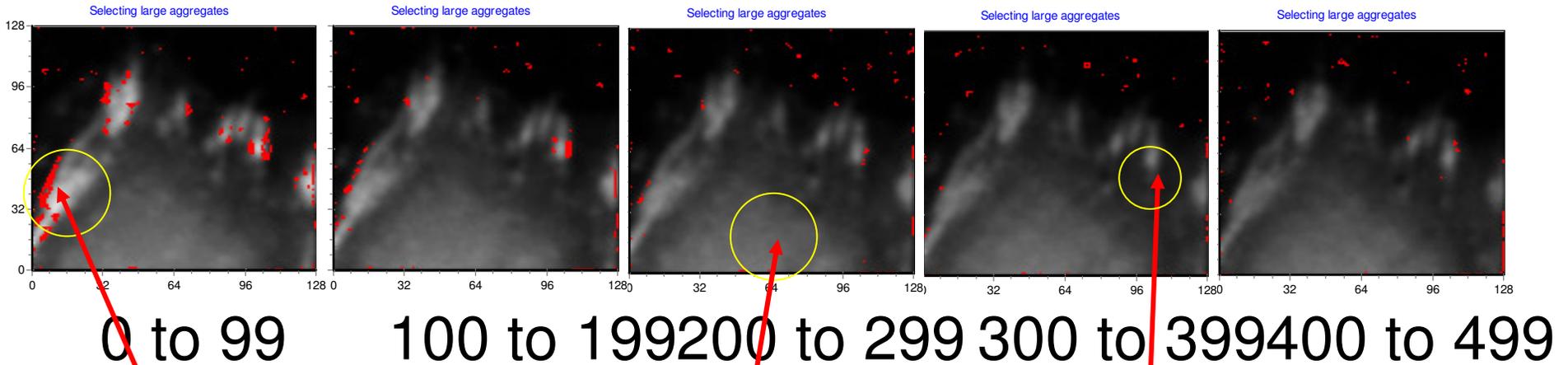
x= 1.88378 y= 1.27400 #pixels= 716 in= 1



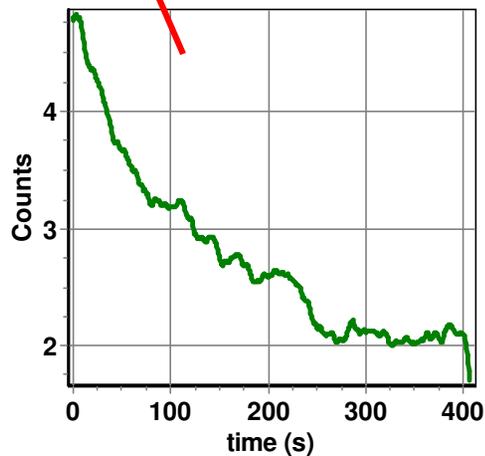
Selected Monomers Selected >5mers

Assembly and disassembly occurs in the order of minutes

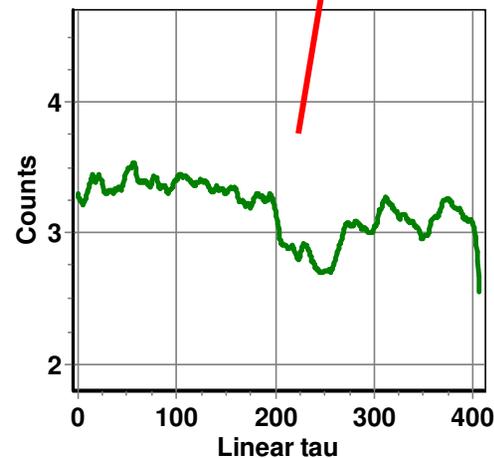
100 Frame average \bar{S} Selecting large aggregates



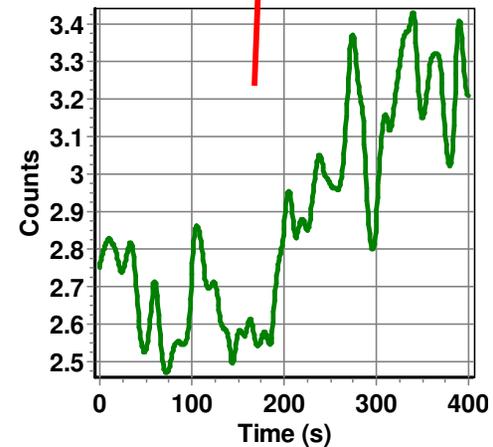
pixel 6,89 average intensity in a region 8x8



pixel 67,120 Intensity change in a 8x8 region



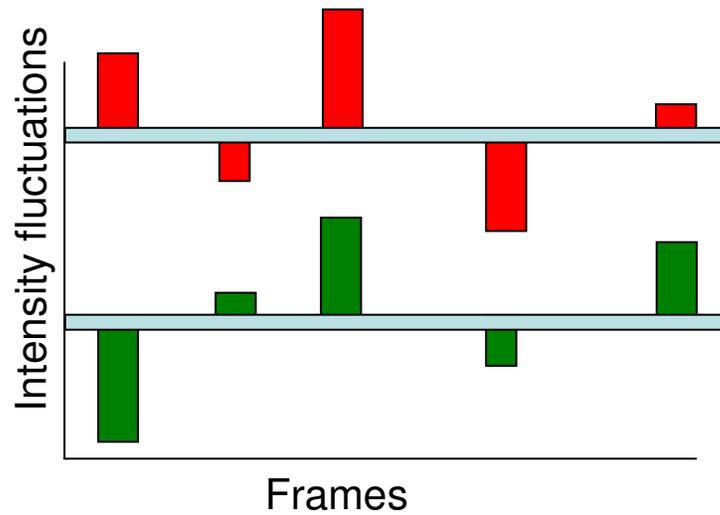
pixel 104,68 A= 0.00000 k= 0.00000 B= 0.00000



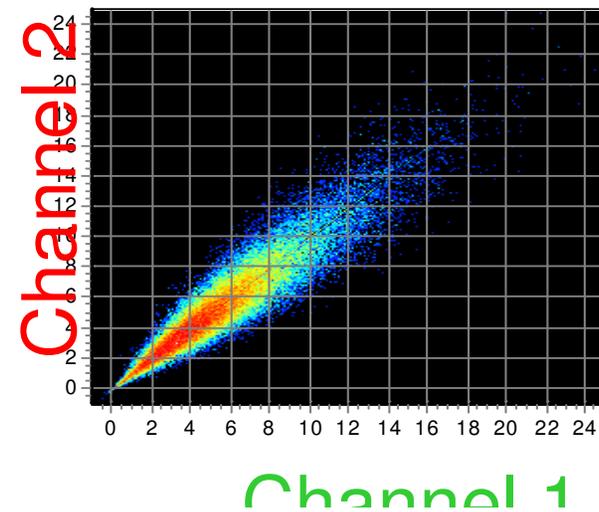
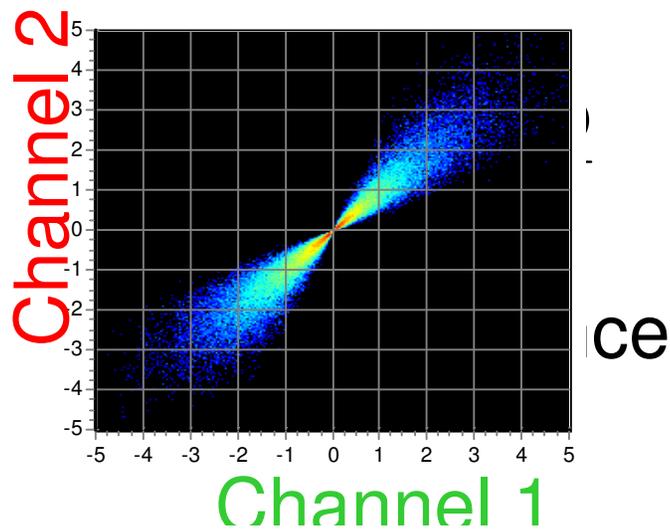
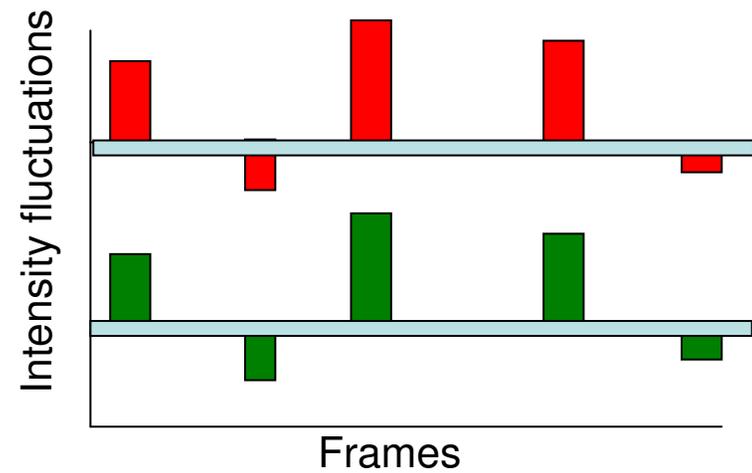
Cross N&B

Conceptual illustration of Cross N&B

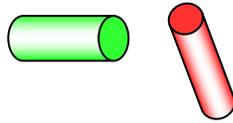
Uncorrelated



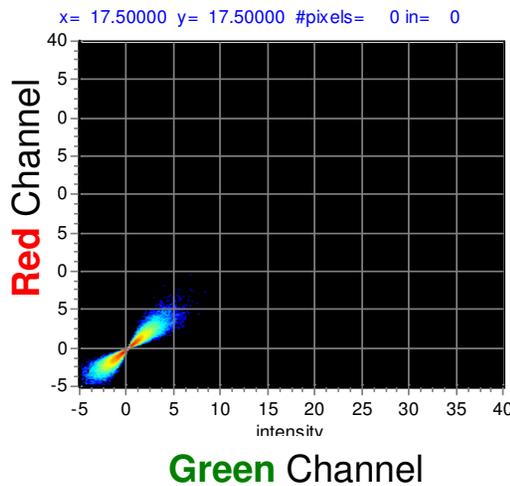
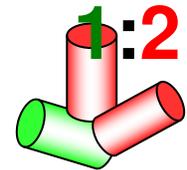
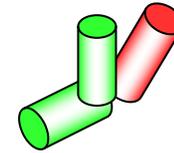
Correlated



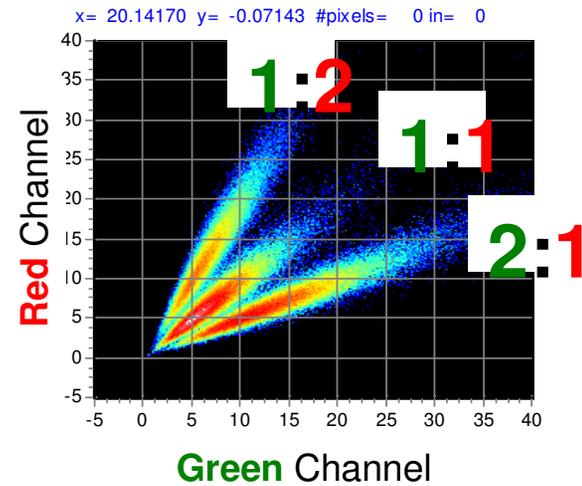
Cross N&B Analysis determines stoichiometry



1:1
2:1



No Cross-Brightness



Positive Cross-Variance

This example is only for ideal systems where the brightness is calibrated for both channels.

The co-variance principle and the derivation of the ccN&B method

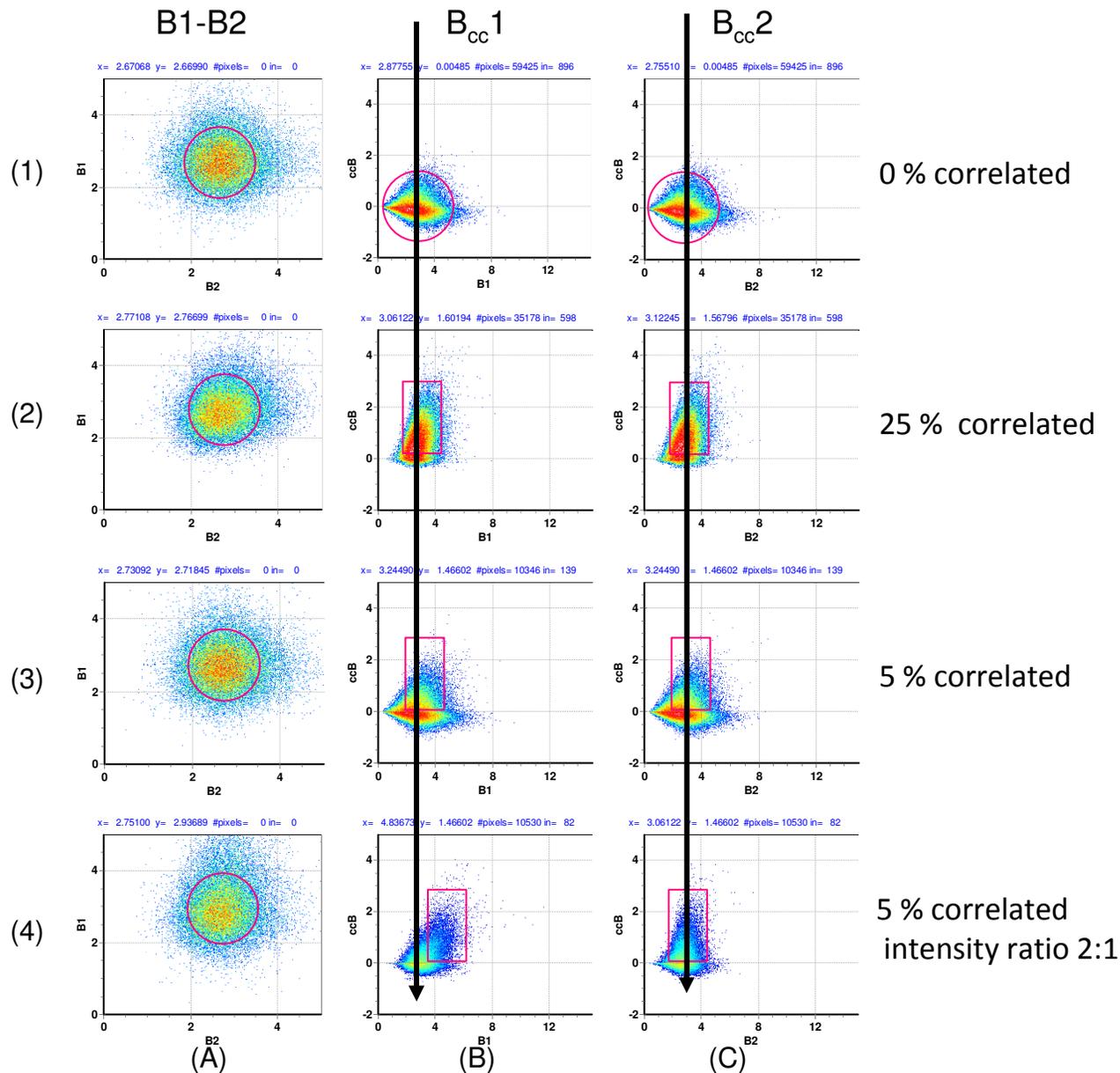
$$\sigma_{cc}^2 = \frac{\sum (G_i - \langle G \rangle)(R_i - \langle R \rangle)}{K}$$

$$N_{cc} = \frac{\langle G \rangle \langle R \rangle}{\sigma_{cc}^2}$$

Definition of co-variance.
It is the average of product of the fluctuations in the Green and Red channel
Definition of the cross-number of molecules. It is the co-variance divided by the product of the intensity in the two channels

K is the number of frames. σ^2 the variance and $\langle \rangle$ indicate

To calibrate the system we need to know the brightness of the monomers



1) calibrate the monomers in both channels The lack of symmetry is due to Poissonian rather than Gaussian distribution of counts

2) Add correlated molecules (still all monomers)

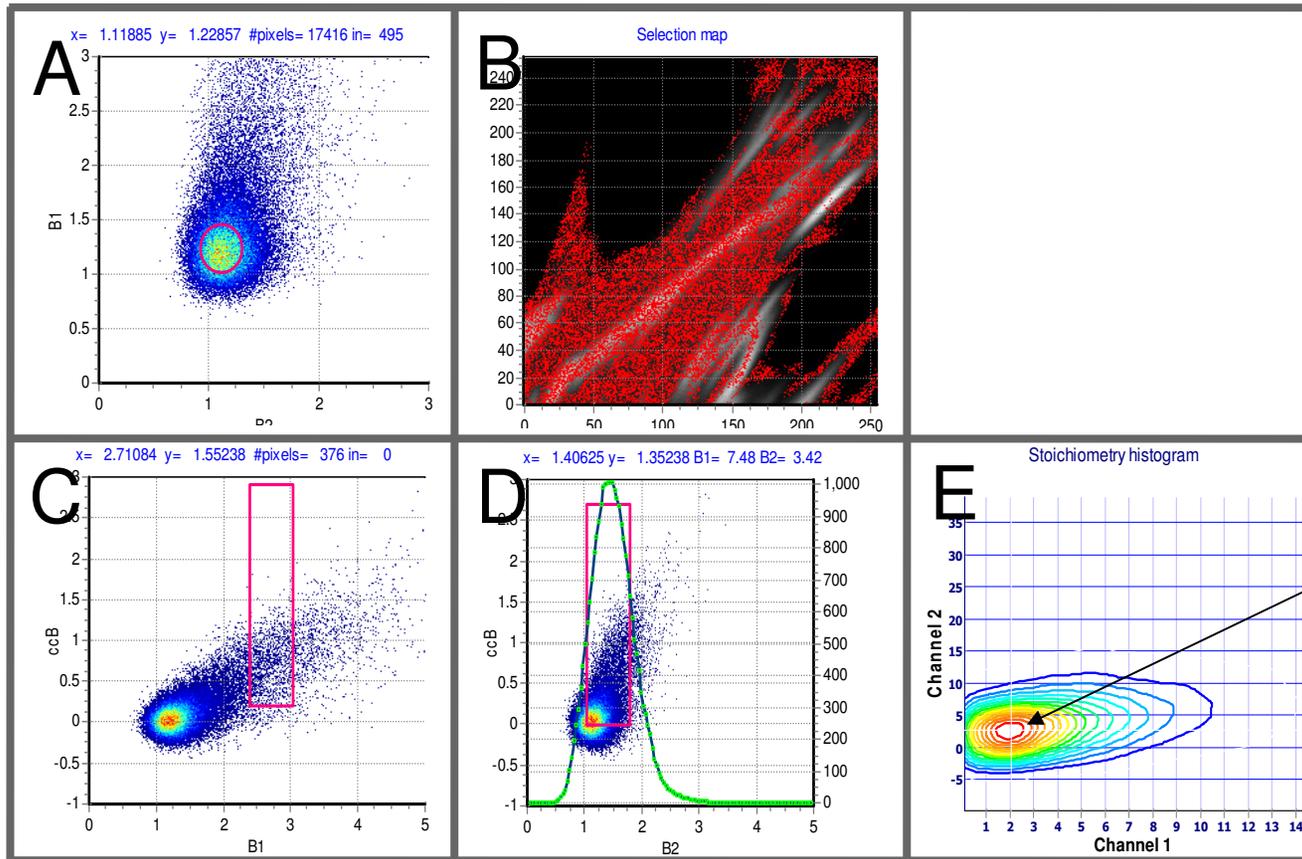
3) At 5% you can still distinguish the positive correlated fluctuations

4) Now we have 2:1 stoichiometry. We have more brightness in B1 but the same in B2

What to look for:

- 1) First we need to calibrate the monomers
- 2) We have to see if there is positive cross variance
- 3) We have to see where the cross variance occurs in respect to the brightness of Ch1 and Ch2

The unknown sample: Vinculin-EGFP and Paxillin-mcherry

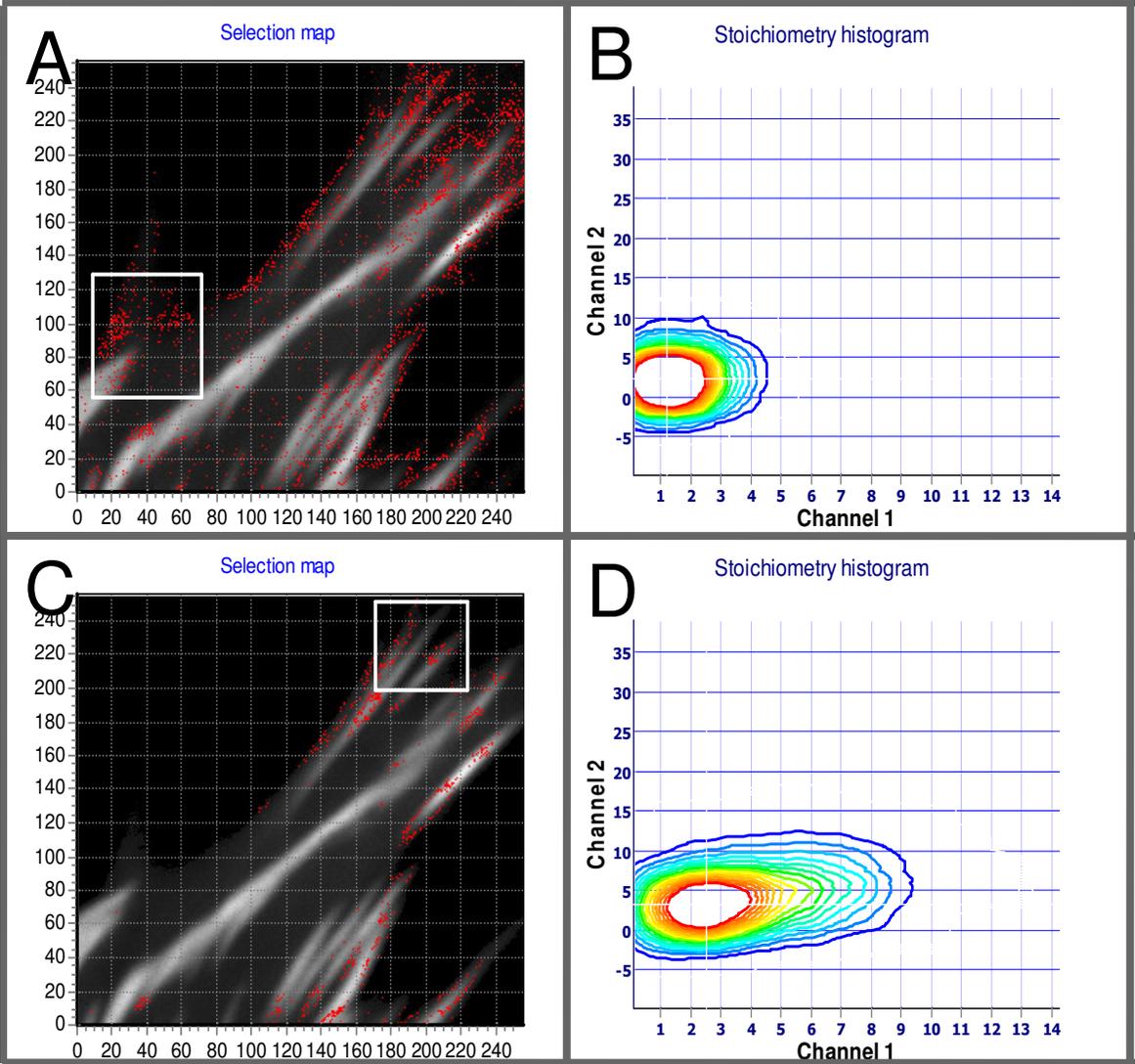


2:3

Look at the brightnesses that coincide for Ch1 a

We must find for each value of B1 in one pixel, what is the
The fluctuations must be correlated so we only look at th

Selecting different regions of the image



Slide 62

AFH1

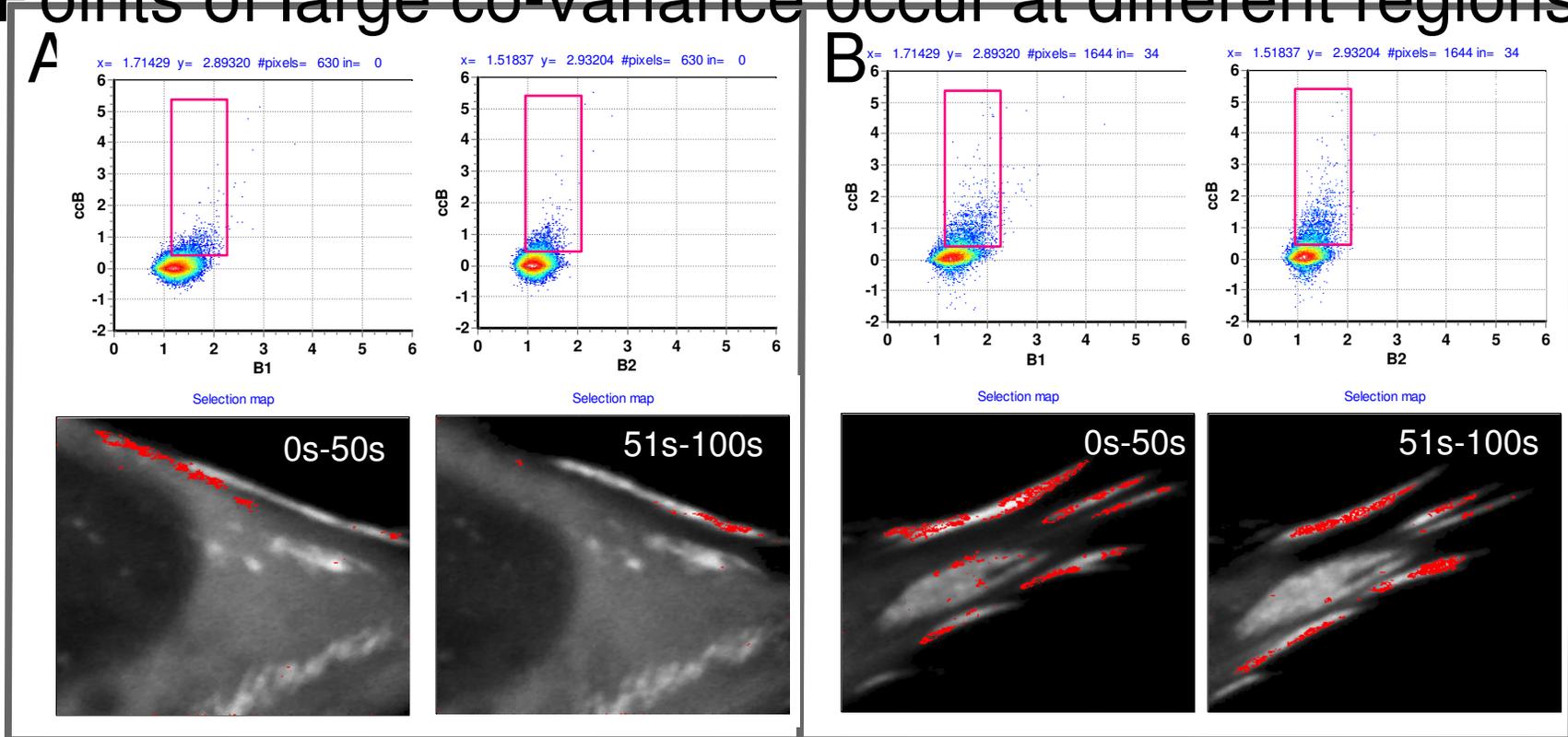
Make sure I didnt mess this up.

Rick Horwitz, 6/18/2008

Cross-correlations occur at specific pixels at the adhesions

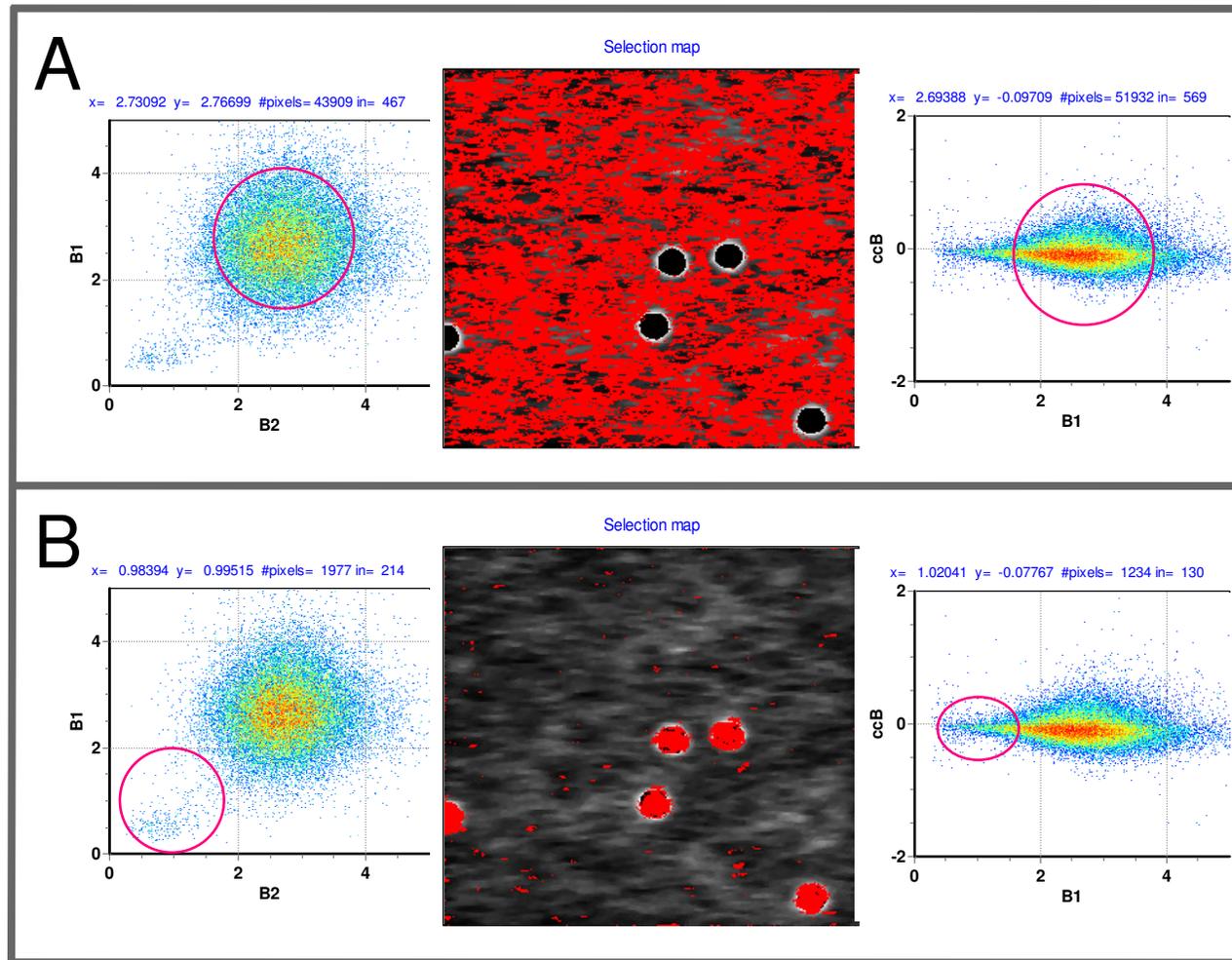
Vinculin-EGFP and Paxillin-mcherry

1. Large Cross variance is only seen at the adhesion
2. Points of large co-variance occur at different regions an



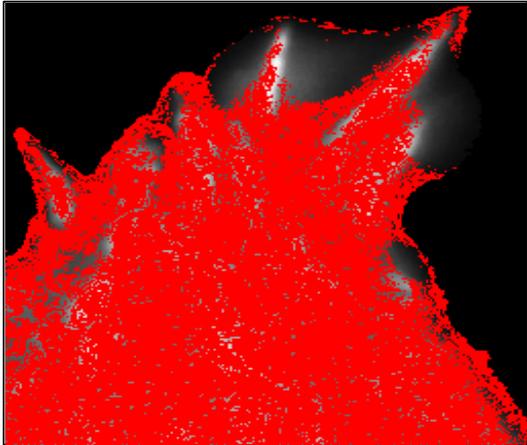
We determined that the brightness for monomers B1= 1.118 and B2=1.22. Thus the ccB1= 6x monomer and for ccB2= 3 x the monomer

Simulations: effect of bright immobile features

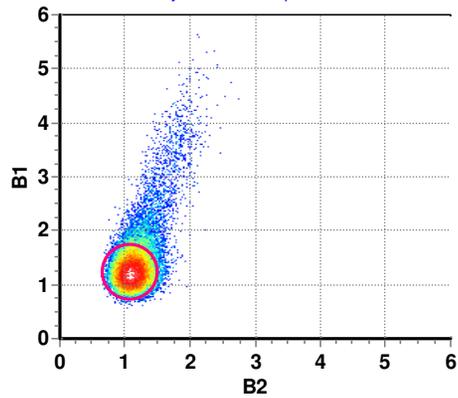


FAK and Paxillin

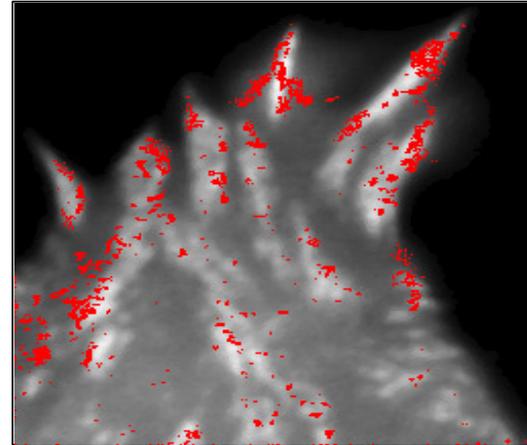
Selection map



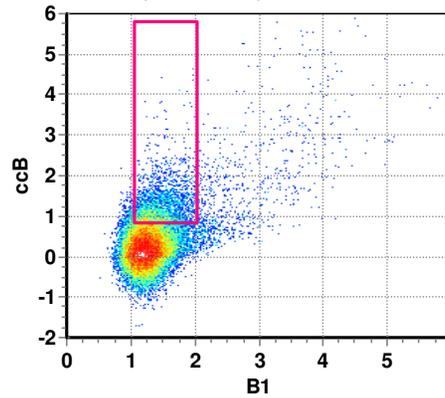
x= 1.08434 y= 1.21053 #pixels= 37301



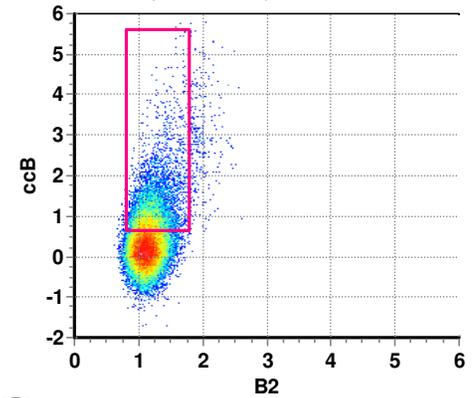
Selection map



x= 1.54286 y= 3.32039 #pixels= 2699 in= 18



x= 1.30120 y= 3.14286 #pixels= 2699 in= 18

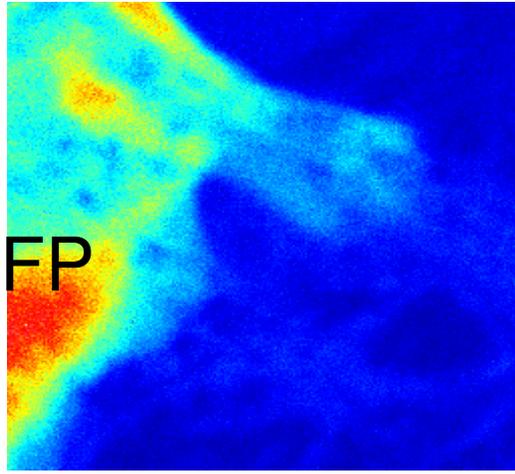


3:4

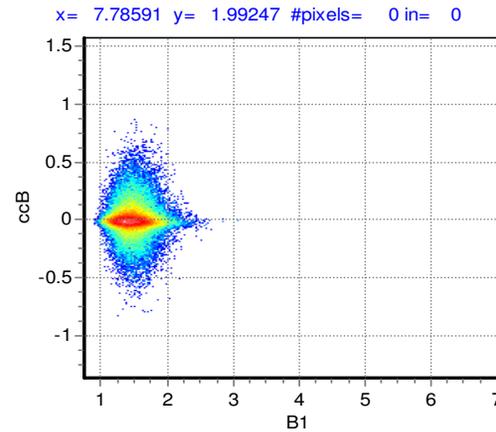
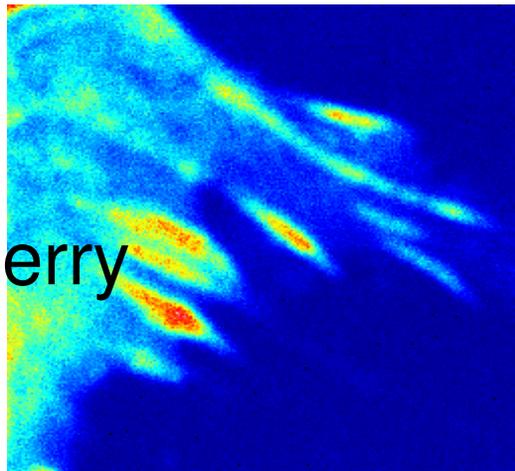


Testing for artifacts: FAK mutant does not form complexes

FAK-EGFP



Pax-mCherry



mutFAK-PAX cell shows no cross-correlation although the cell
forms a strong focal adhesion (FAK)

Summary

- N&B distinguishes between number of molecules and molecular brightness in the same pixel
- The acquisition for the N&B can be done with a commercial Laser Scanning Microscope (LSM) and the same data used for RICS can be used to map N and B.
- The Immobile fraction can be separated since it has a Brightness value =1
- The N&B analysis of paxillin at adhesions shows large aggregates of protein during disassembly.
- Cross N&B allows us to determine the stoichiometry of the complexes.

Additional Reading

- 1) Jay R Unruh and Enrico Gratton. Analysis of molecular concentration and brightness from fluorescence fluctuation data with an electron multiplied CCD camera. *Biophys J.* 2008; [epub ahead of print].
- 2) Michelle A Digman, Rooshin Dalal, Alan R Horwitz, and Enrico Gratton. Mapping the number of molecules and brightness in the laser scanning microscope. *Biophys J.* 2008; 94(6): 2320-2332.
- 3) Rooshin B Dalal, Michelle A Digman, Alan R Horwitz, Valeria Vetri, and Enrico Gratton. Determination of particle number and brightness using a laser scanning confocal microscope operating in the analog mode. *Microsc Res Tech.* 2008; 71(1): 69-81.
- 4) Yan Chen, Joachim D Müller, Qiaoqiao Ruan, and Enrico Gratton. Molecular brightness characterization of EGFP in vivo by fluorescence fluctuation spectroscopy. *Biophys J.* 2002; 82(1): 133-44.
- 5) Alberto Garcia-Marcos, Susana A Sánchez, Pilar Parada, John S Eid, David M Jameson, Miguel Remacha, Enrico Gratton, and Juan P G Ballesta. Yeast ribosomal stalk heterogeneity in vivo shown by two-photon FCS and molecular brightness analysis. *Biophys J.* 2008; 94(7): 2884-2890.
- 6) Michelle A Digman, Paul W Wiseman, Colin K Choi, Alan R Horwitz, and Enrico Gratton. Mapping the stoichiometry of molecular complexes at adhesions in living cells. *Proc Natl Acad Sci USA.* 2008; [submitted].